Morphometrics with SPM12

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What kind of differences are we looking for?

- Usually, we try to localise regions of difference.
  - **Univariate models**.
  - Typically involves fitting a GLM
  - Typically localising volumetric differences
- Some anatomical differences can not be localised.
  - Need **multivariate models**.
  - Differences in terms of proportions among measurements.
  - Where would the difference between male and female faces be localised?
- Need to select the best model of difference to use, before trying to fill in the details.

Overview

- **Voxel-Based Morphometry**
- Diffeomorphic Registration
- Tensor-Based Morphometry
- Longitudinal Registration

Voxel-Based Morphometry

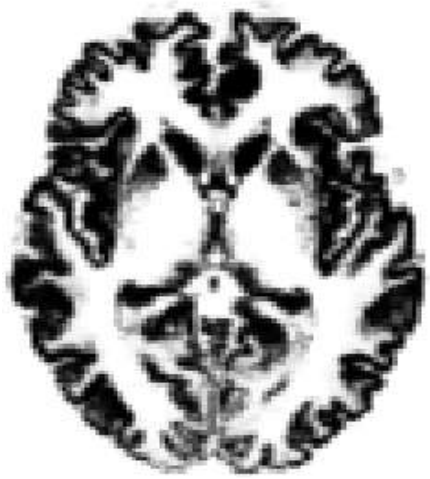
- Produce a map of statistically significant differences among populations of subjects.
  - e.g. compare a patient group with a control group.
  - or identify correlations with age, test-score etc.
- The data are pre-processed to sensitise the tests to regional tissue volumes.
  - Usually grey or white matter.

Volumetry

T1-Weighted MRI

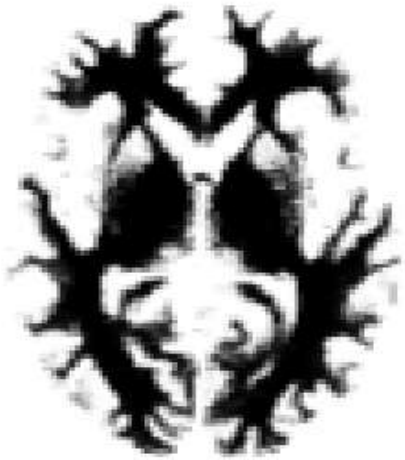
Grey Matter

Original

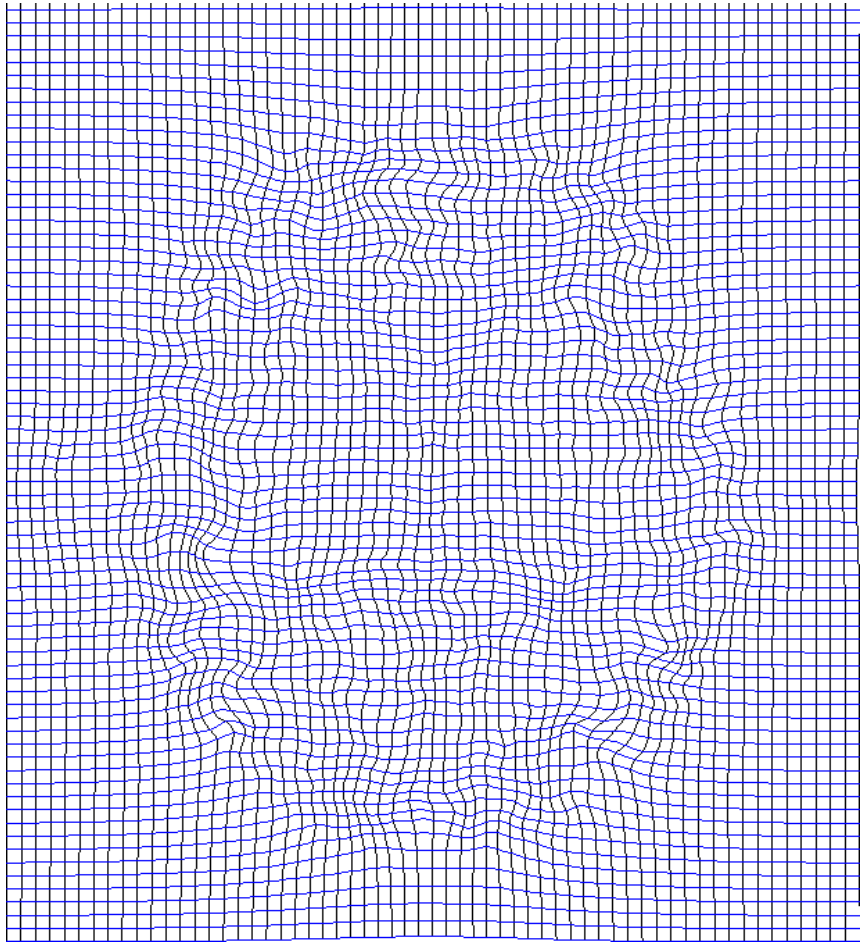


Warped

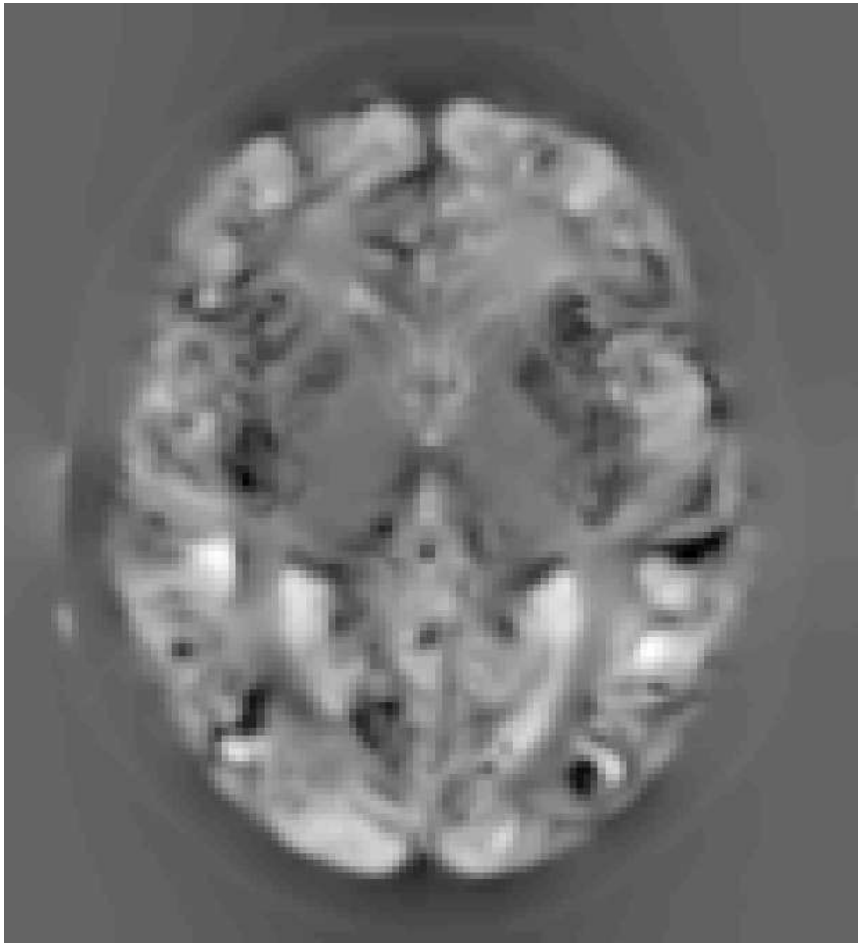
Template



“Modulation” – change of variables.



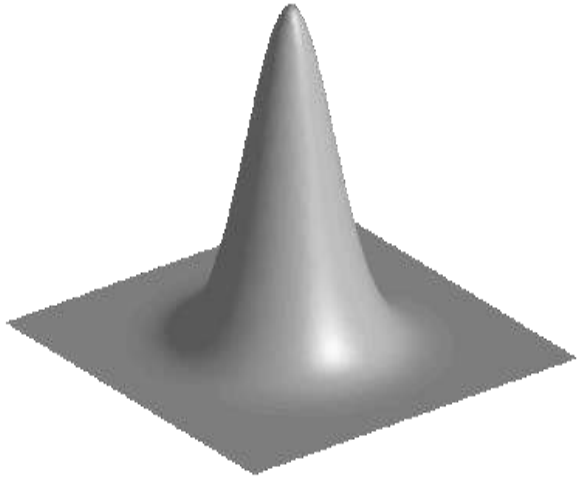
Deformation Field



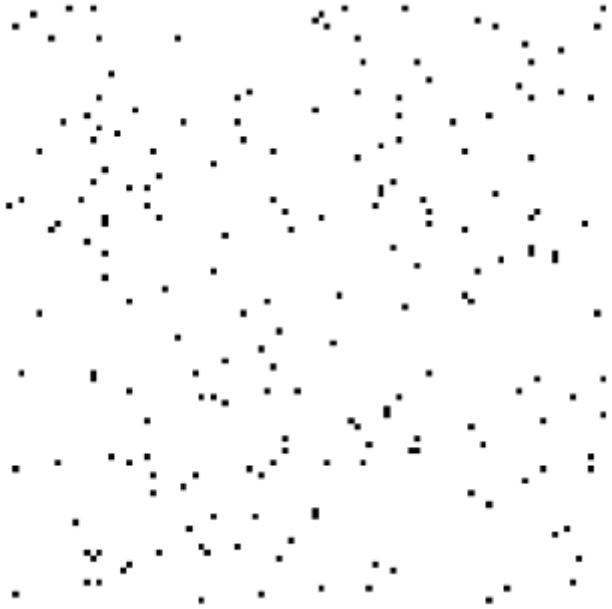
Jacobians determinants
Encode relative volumes.

Smoothing

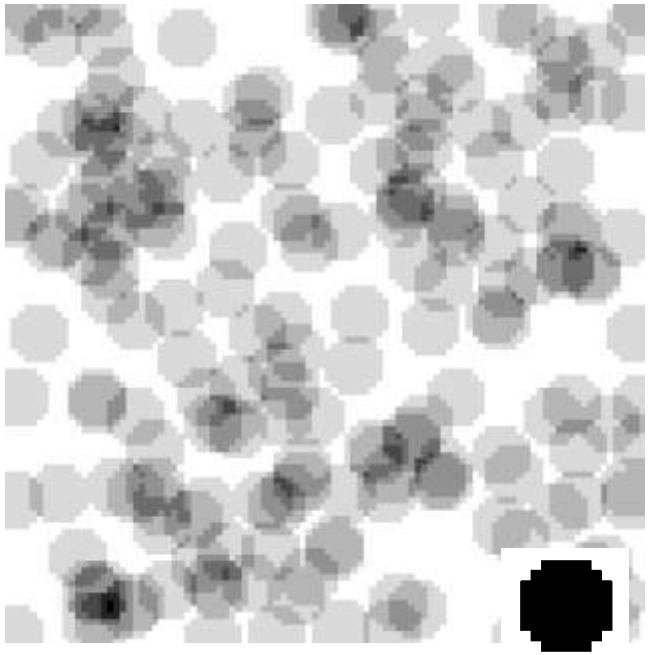
Each voxel after smoothing effectively becomes the result of applying a weighted region of interest (ROI).



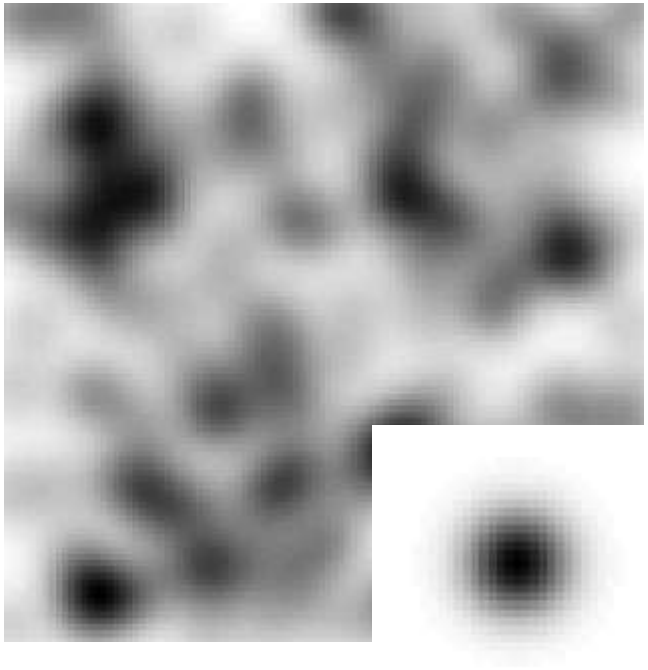
Before convolution



Convolved with a circle

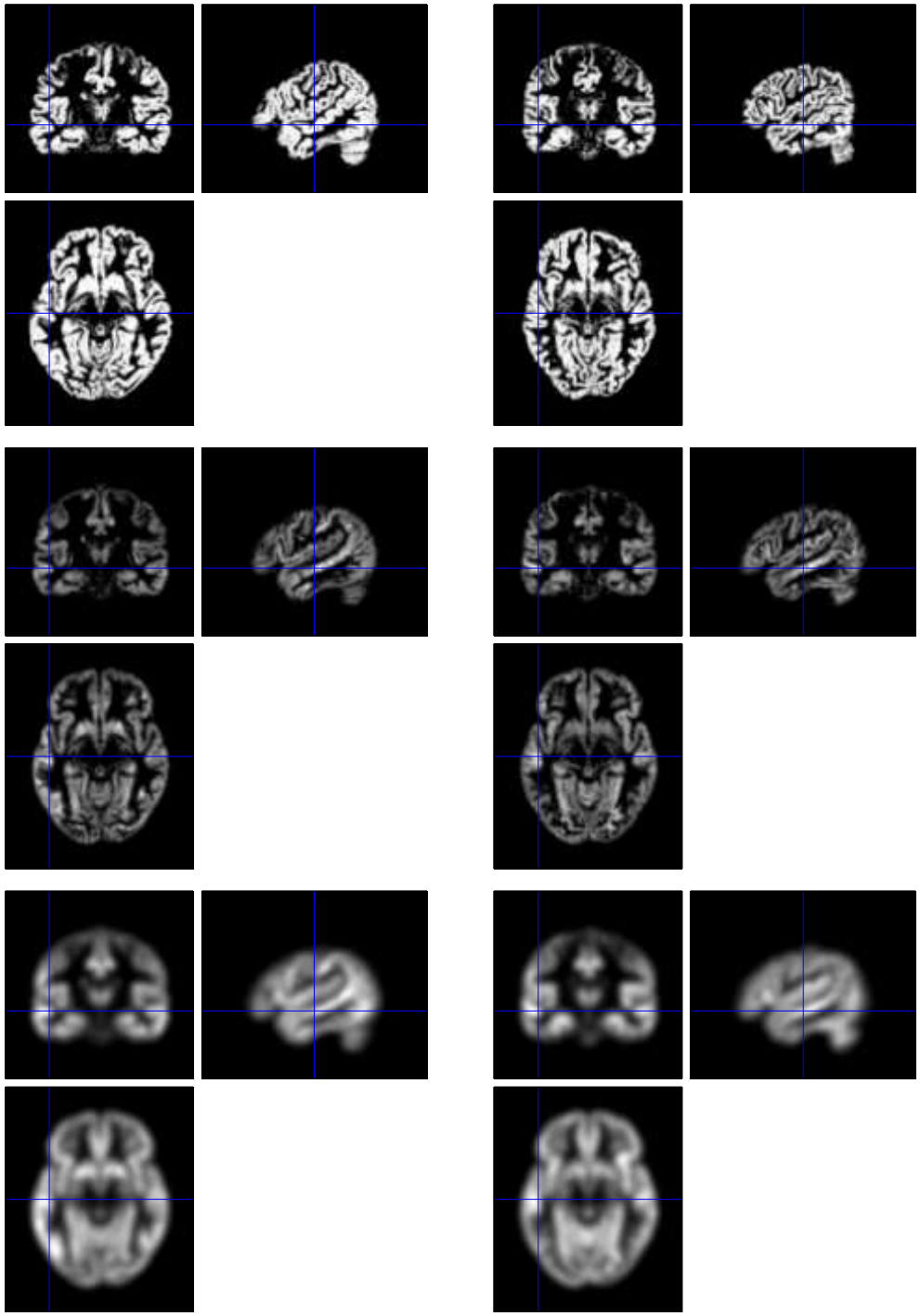


Convolved with a Gaussian

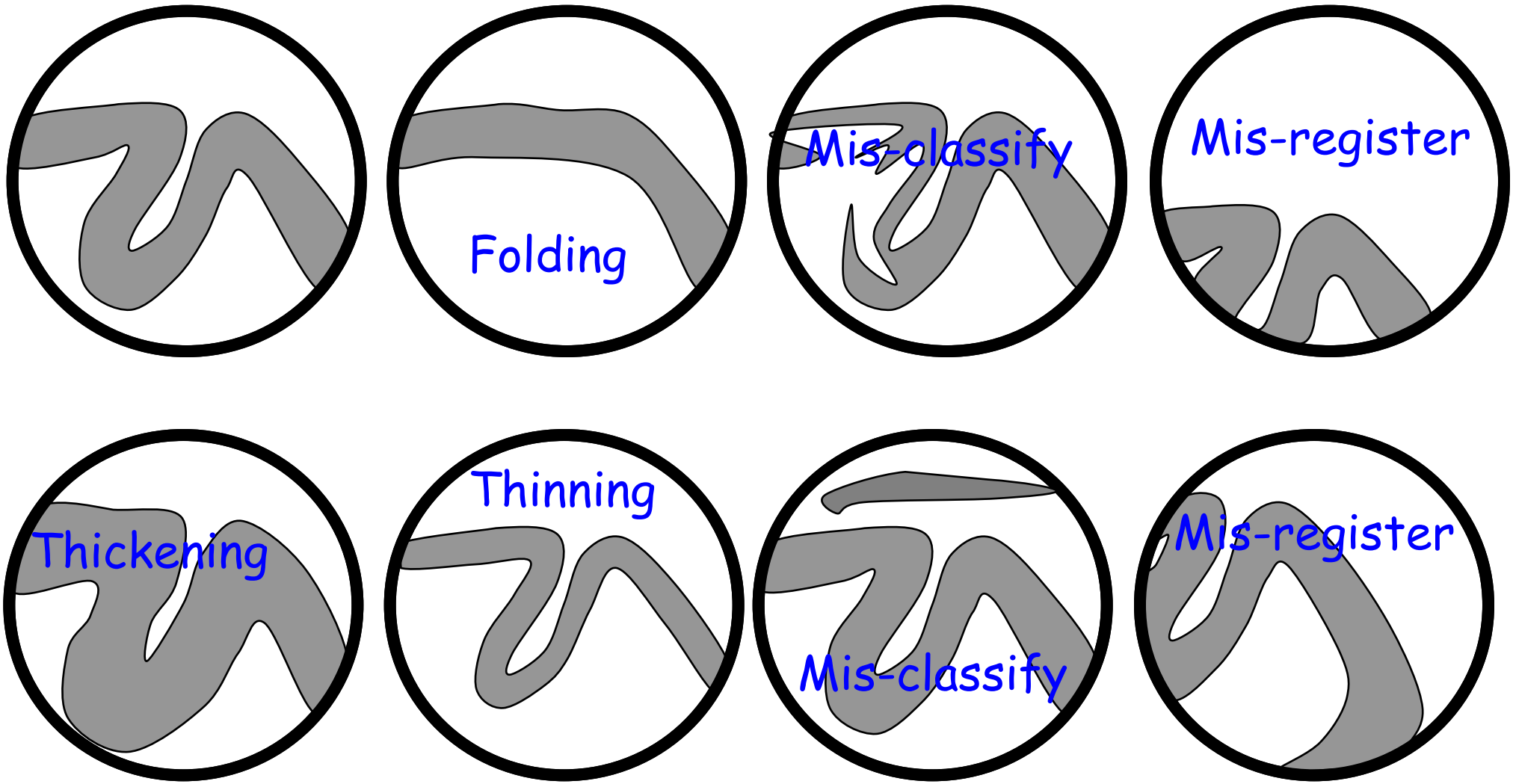


VBM Pre-processing in SPM12

- Use Segment for characterising intensity distributions of tissue classes, and writing out “imported” images that *Dartel* can use.
- Run *Dartel* to estimate all the deformations.
- *Dartel* warping to generate smoothed, “modulated”, warped grey matter.
- Statistics.



Some Explanations of the Differences



Some References

- Ashburner & Friston. "*Unified Segmentation*". NeuroImage **26**:839-851, 2005.
- Ashburner. "*A Fast Diffeomorphic Image Registration Algorithm"*. NeuroImage 38:95-113 (2007).
- Ashburner & Friston. "*Computing Average Shaped Tissue Probability Templates"*. NeuroImage **45**:333-341, 2009.
- Ashburner. "*Computational Anatomy with the SPM software*". Magnetic Resonance Imaging **27**(8):1163-1174, 2009.

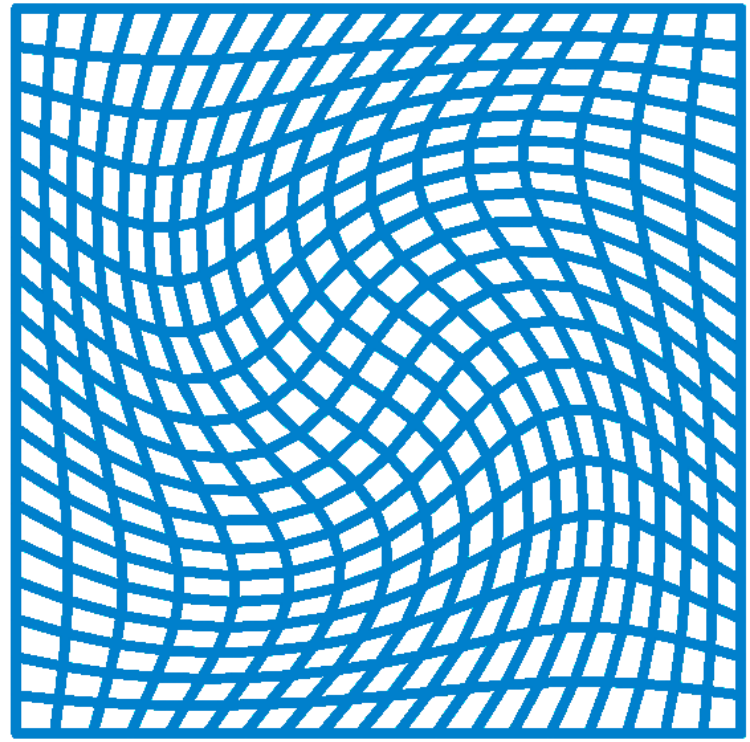
Overview

- Voxel-Based Morphometry
- **Diffeomorphic Registration**
- Tensor-Based Morphometry
- Longitudinal Registration

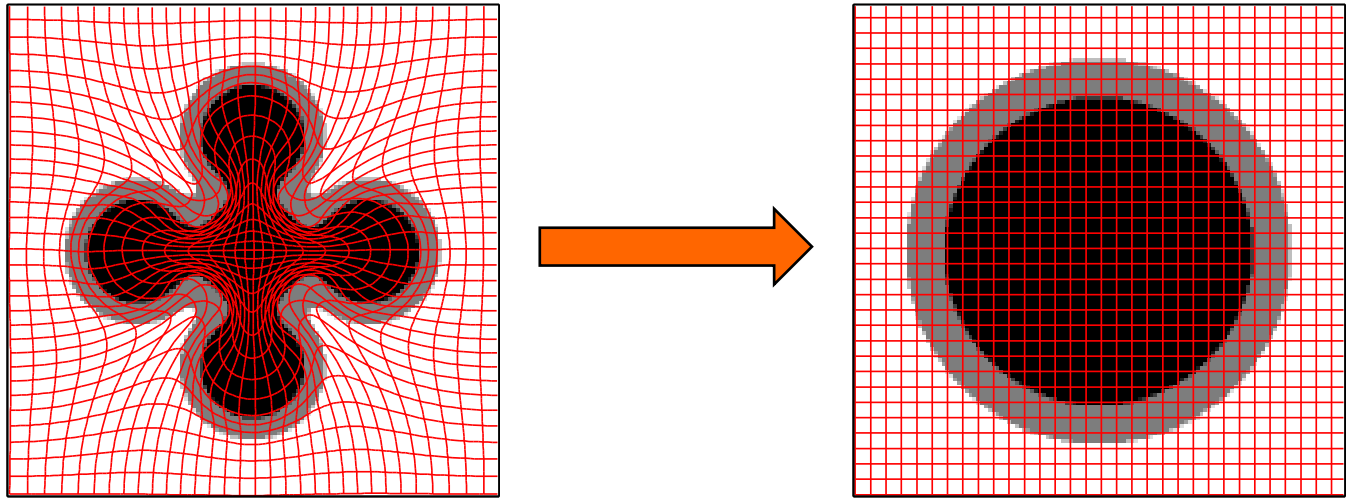
Diffeomorphisn

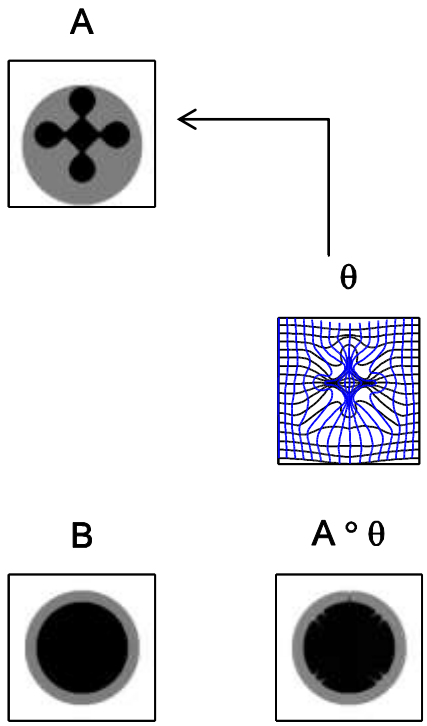
In mathematics, a diffeomorphism is an isomorphism in the category of smooth manifolds. It is an invertible function that maps one differentiable manifold to another, such that both the function and its inverse are smooth.

Wikipedia



Deformations





Composition

Small Deformation Approximation

The composition:

$$\vartheta \circ \varphi$$

Would be approximated with:

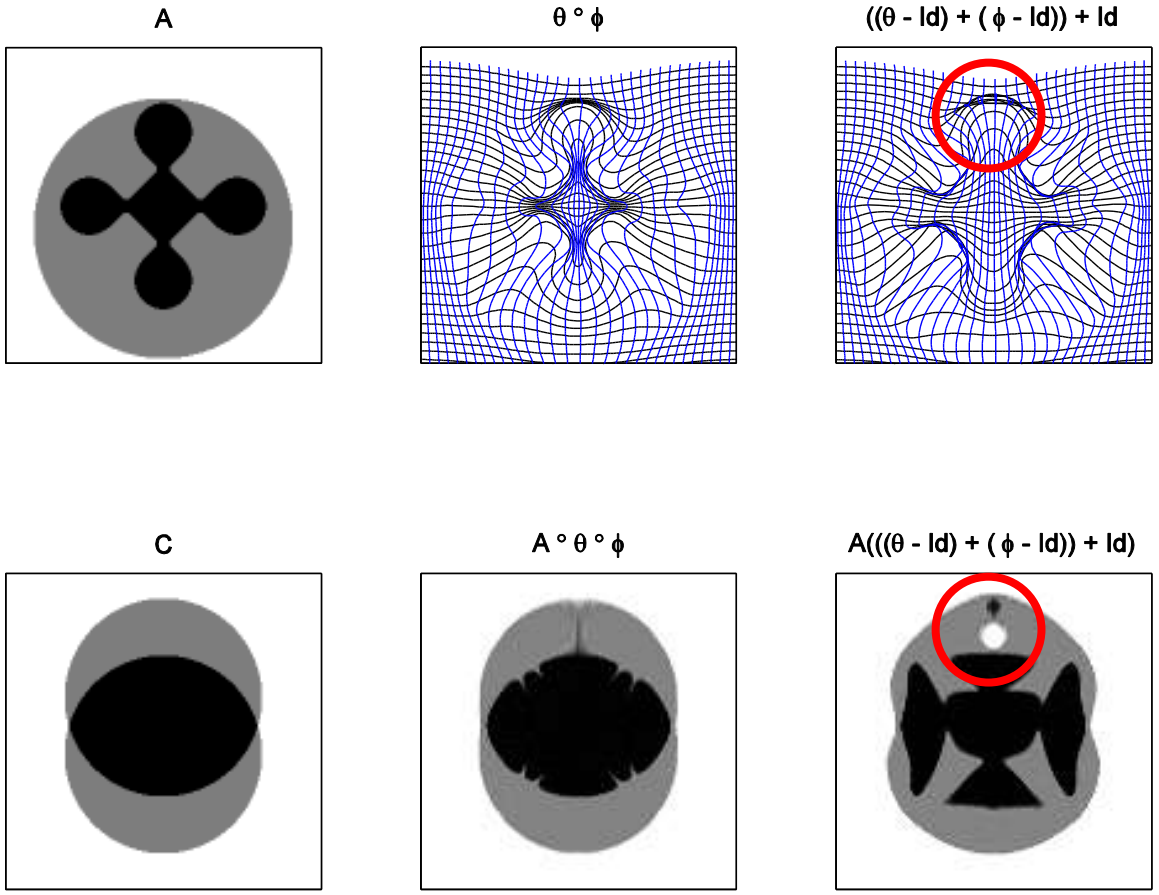
$$Id + ((\vartheta - Id) + (\varphi - Id))$$

The inversion:

$$\varphi^{-1}$$

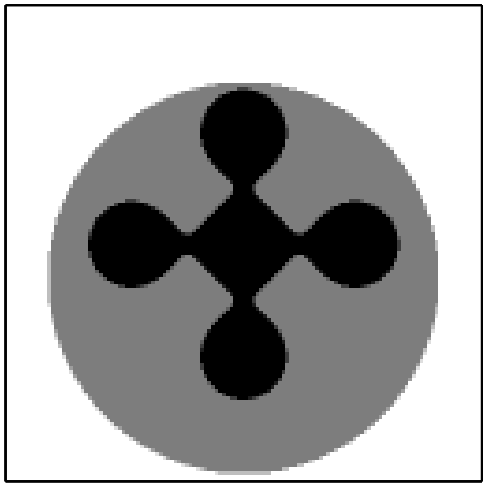
Would be approximated with:

$$Id - (\varphi - Id)$$

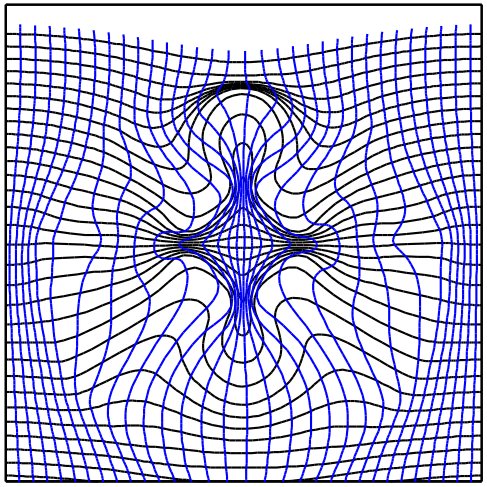


Not good approximations for large deformations.

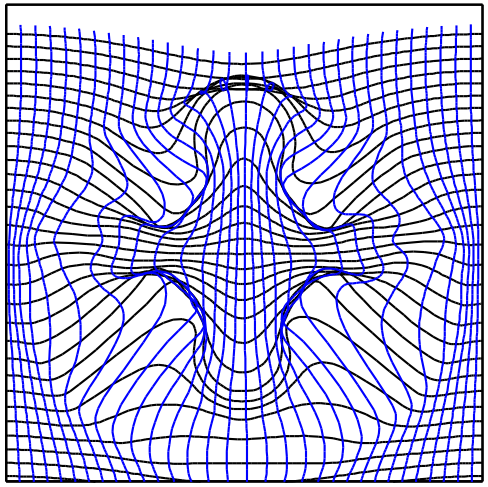
A



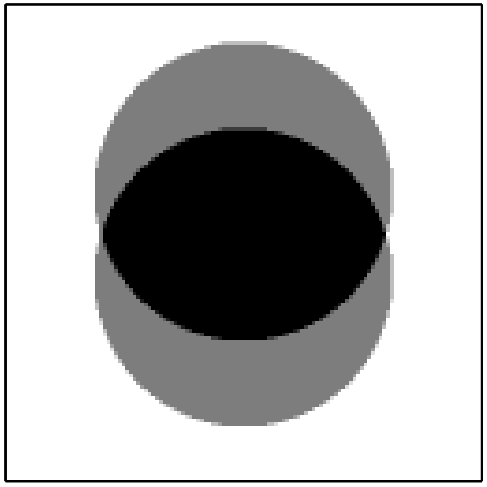
θ ° ϕ



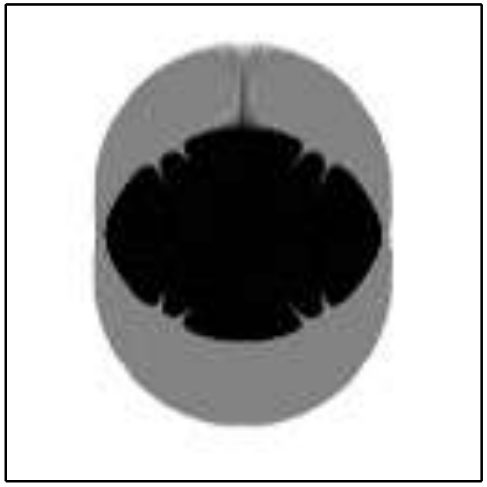
((θ - Id) + (ϕ - Id)) + Id



C



A ° θ ° ϕ



A(((θ - Id) + (ϕ - Id)) + Id)

Diffeomorphic Image Registration

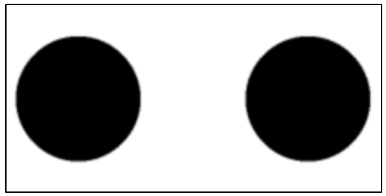
- Minimises two terms:

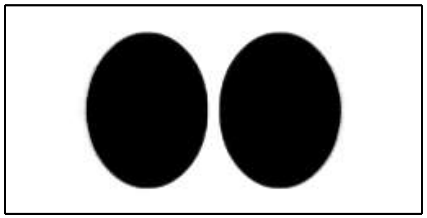
1. A measure of distance between images
2. A measure of the amount of distortion.

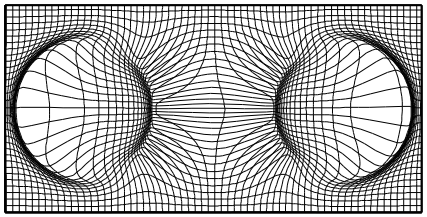
Because we can not simply add displacement fields, large deformations are generated by composing many small deformations.

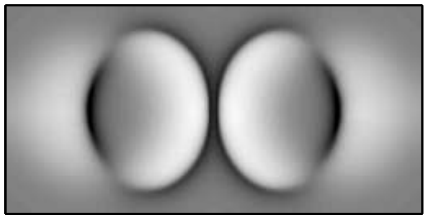
The amount of distortion is computed by summing up the distortion measures from the small displacements.

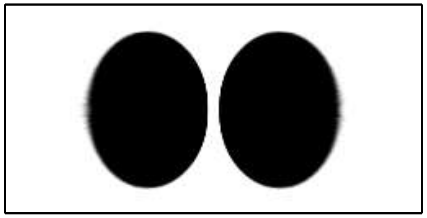
Effect of Different Distortion Measures

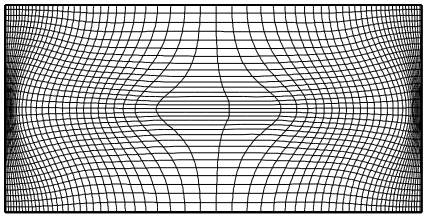


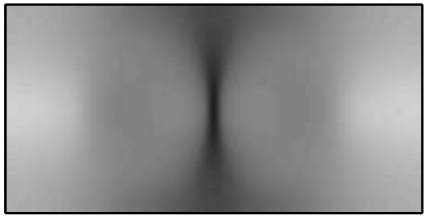


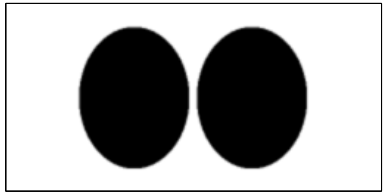


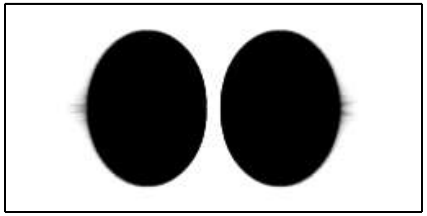


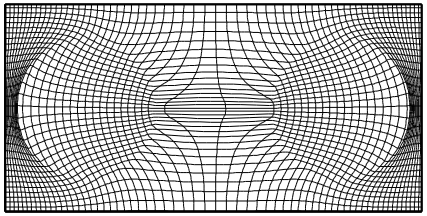


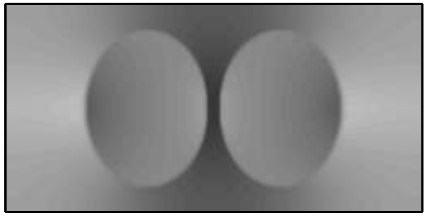


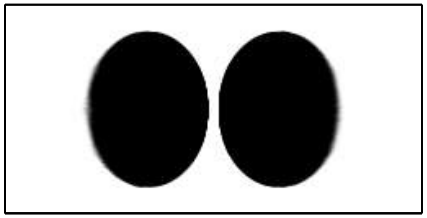


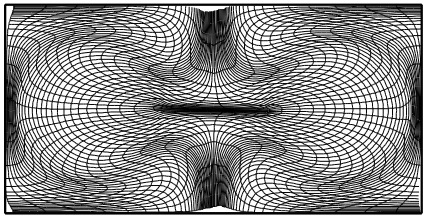


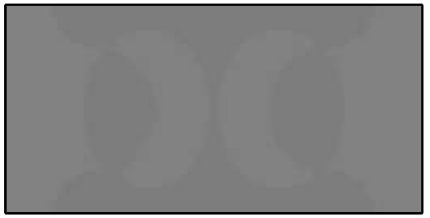












Two diffeomorphic approaches in SPM

Dartel.

- Uses the same small deformation composed multiple times.
- Faster than Geodesic Shooting.
- Gives similar deformations to Geodesic Shooting.
- Currently more additional utilities.

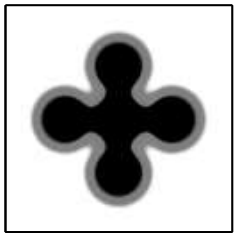
Geodesic Shooting

- Uses the optimal series of small deformations, which are composed together.
- More mathematically correct than Dartel.
- Gives nicer maps of volume change than Dartel.
- Likely to replace Dartel in future.

Dartel & GS Compared

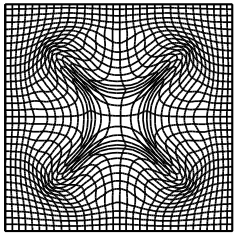
Dartel

$\mu \circ \chi$

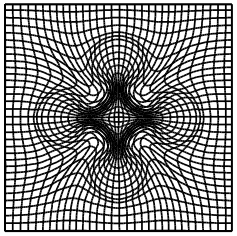


$f \circ \chi^{-1}$

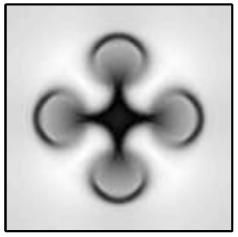
χ



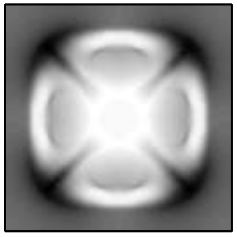
χ^{-1}



$|J^{\chi}|$

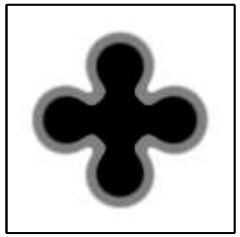


$|J^{\chi^{-1}}|$



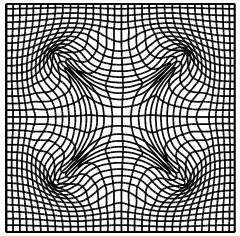
Geodesic Shooting

$\mu \circ \theta$

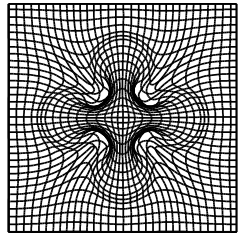


$f \circ \phi$

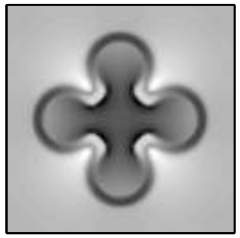
θ



ϕ

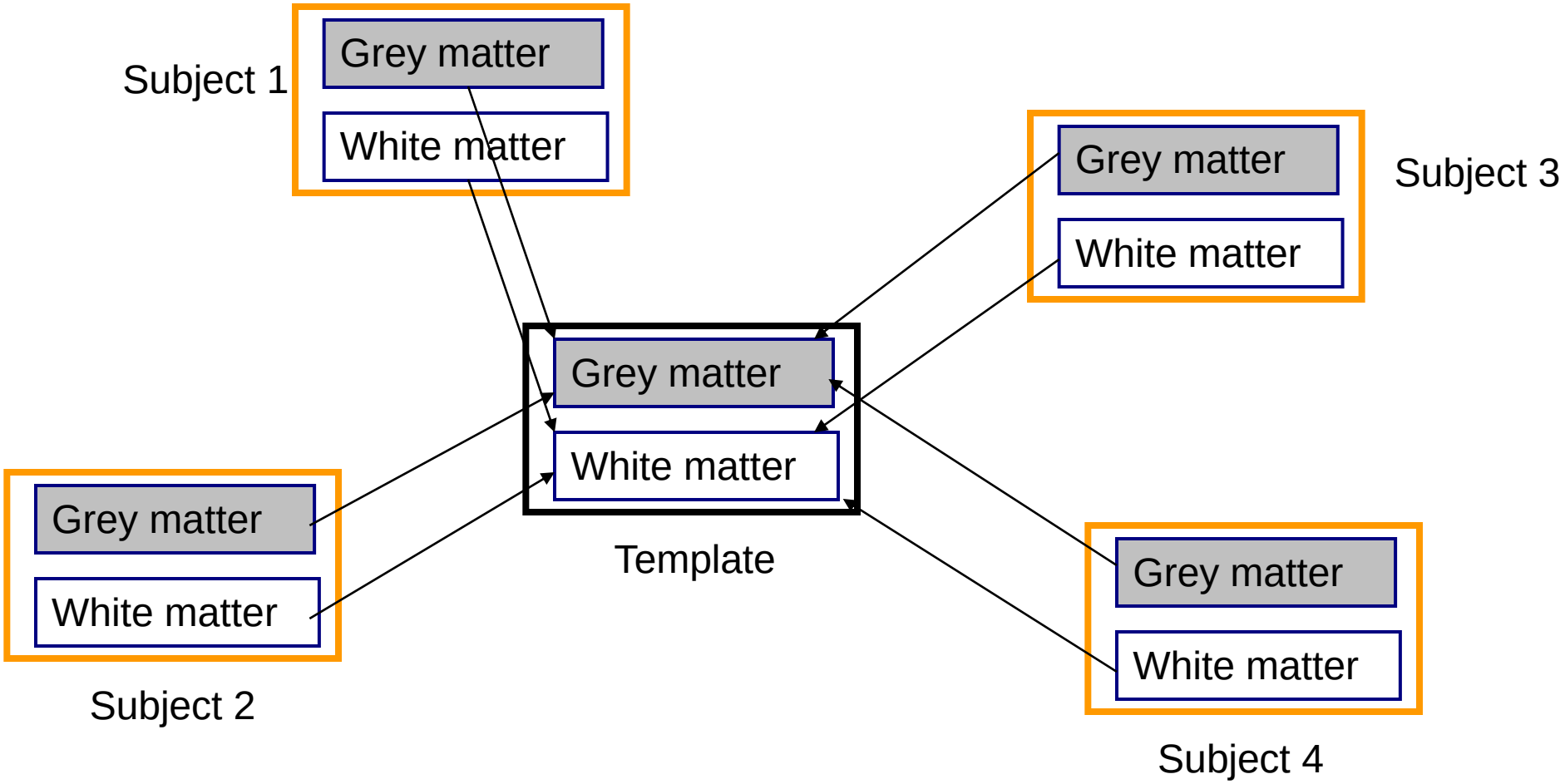


$|J^{\theta}|$



$|J^{\phi}|$

Simultaneous registration of GM to GM and WM to WM

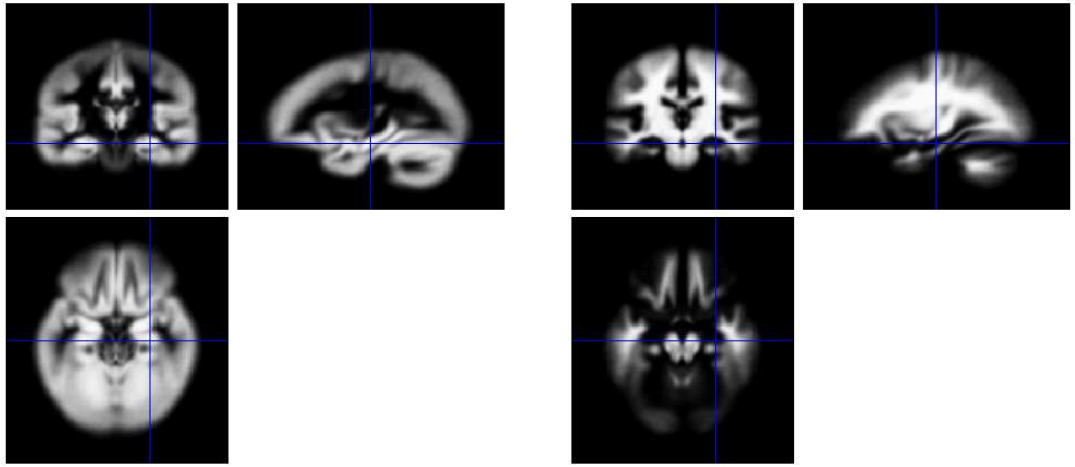


Template

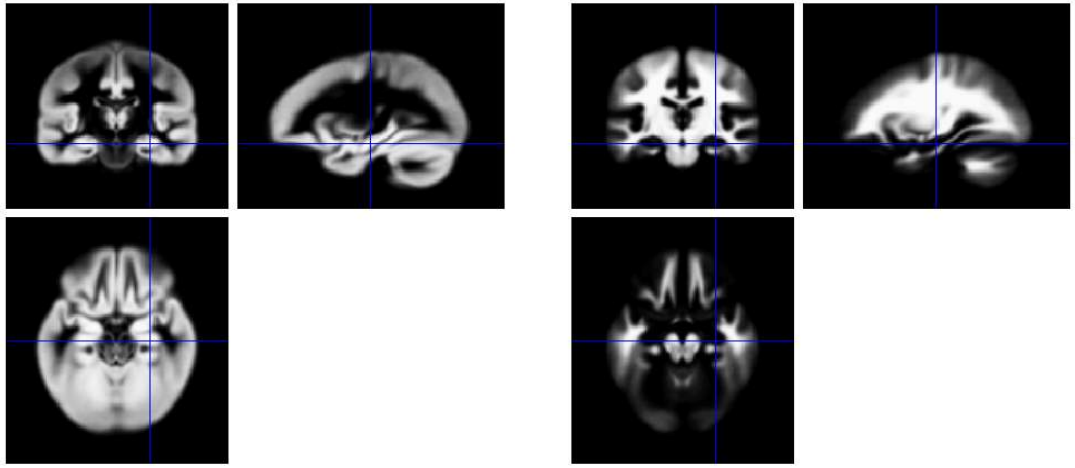
Iteratively generated from all subjects in study

Begin with rigidly aligned tissue probability maps

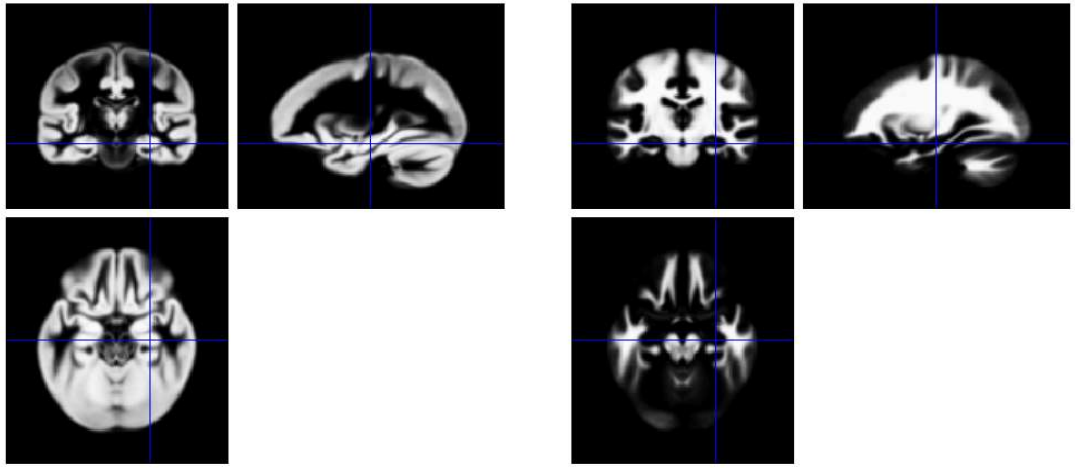
Initial Average



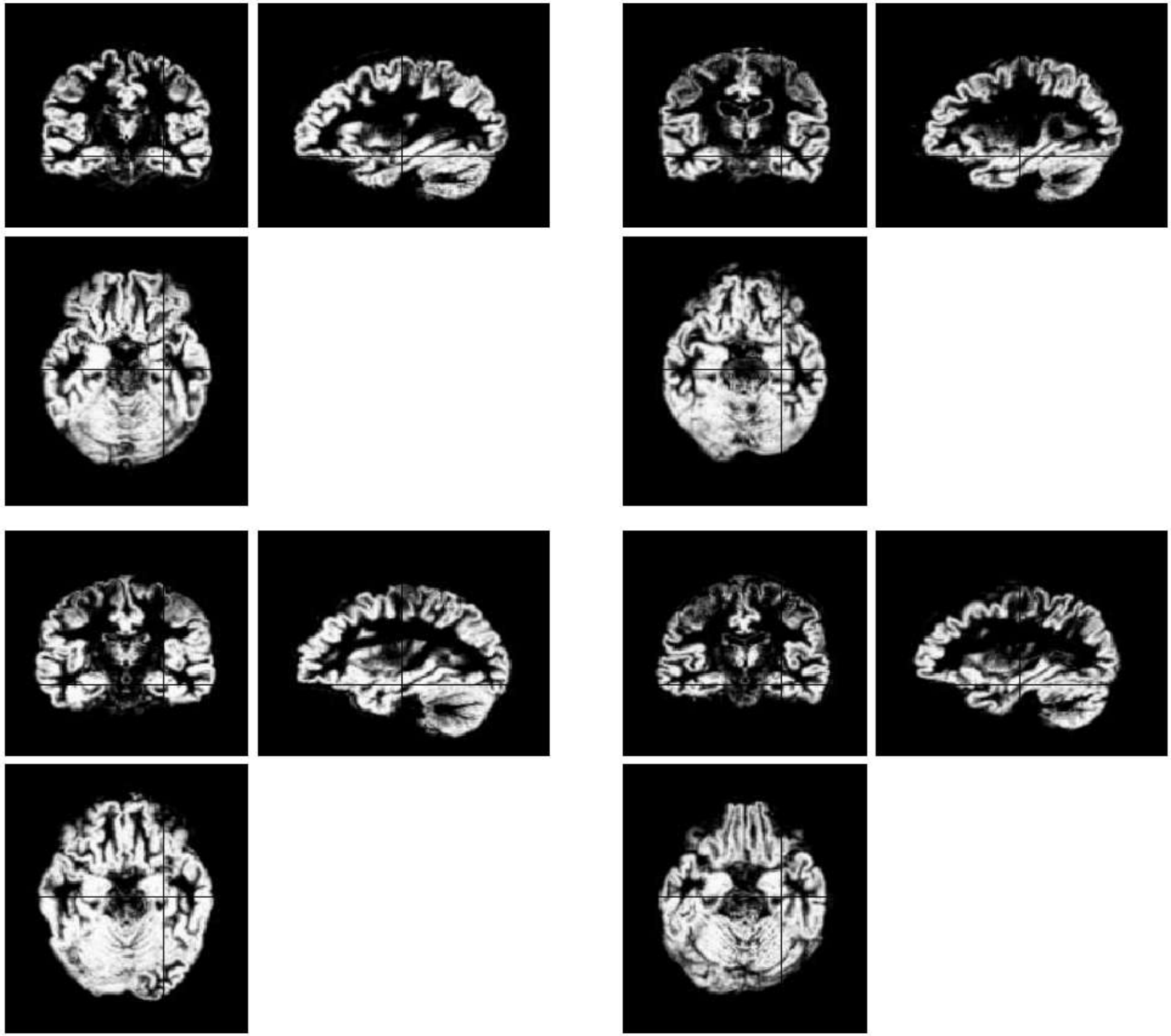
After a few iterations



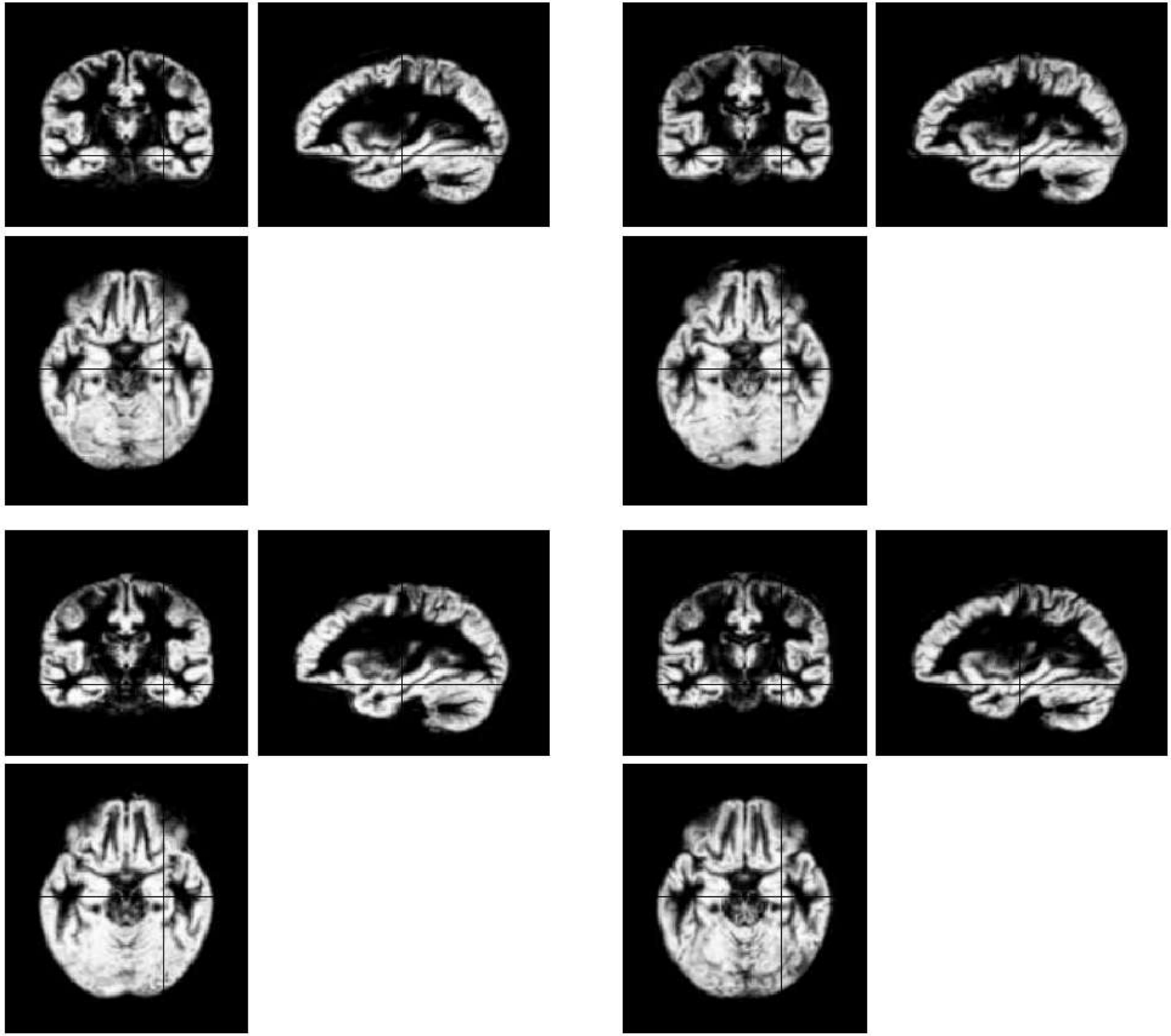
Final template

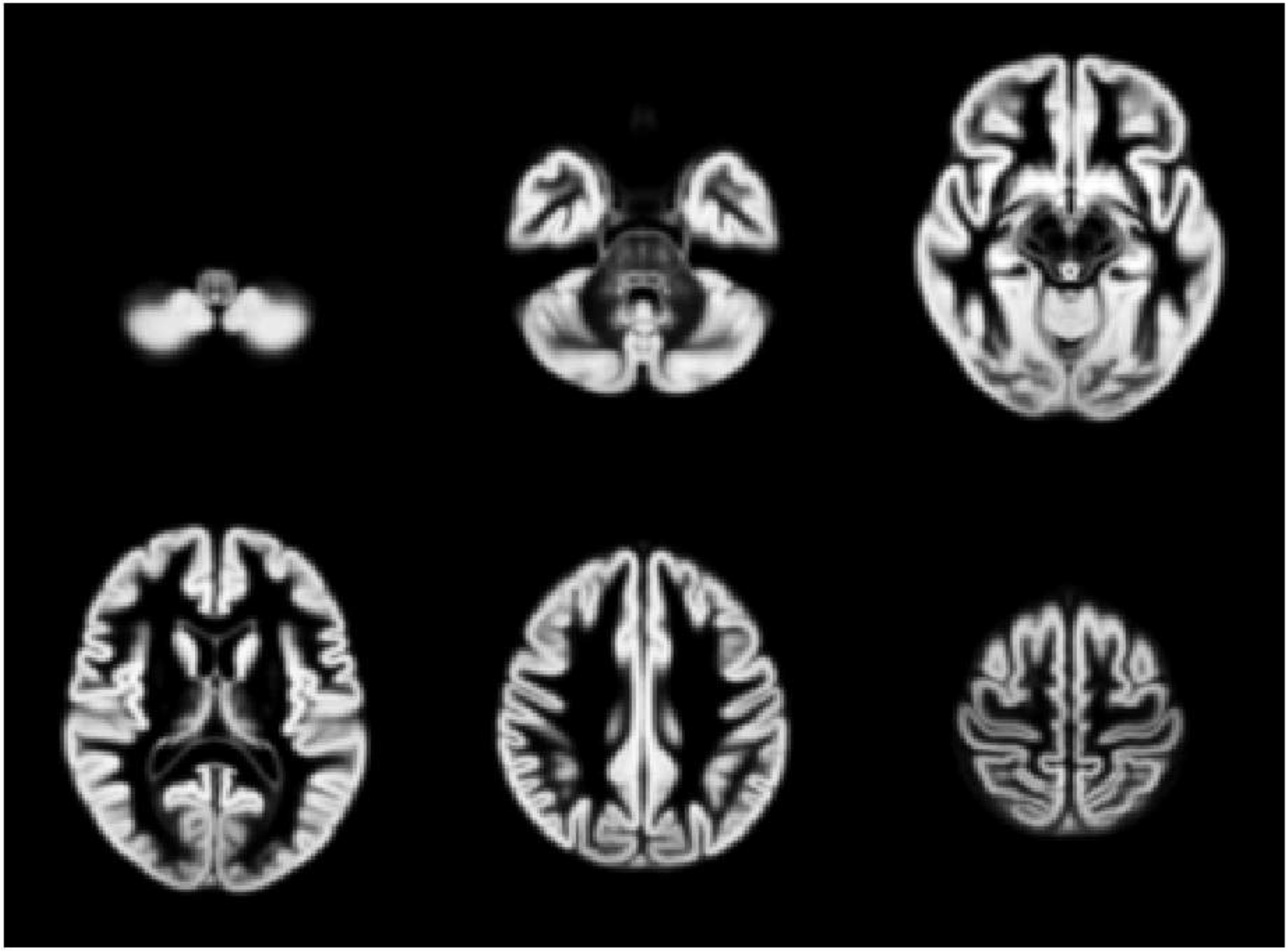


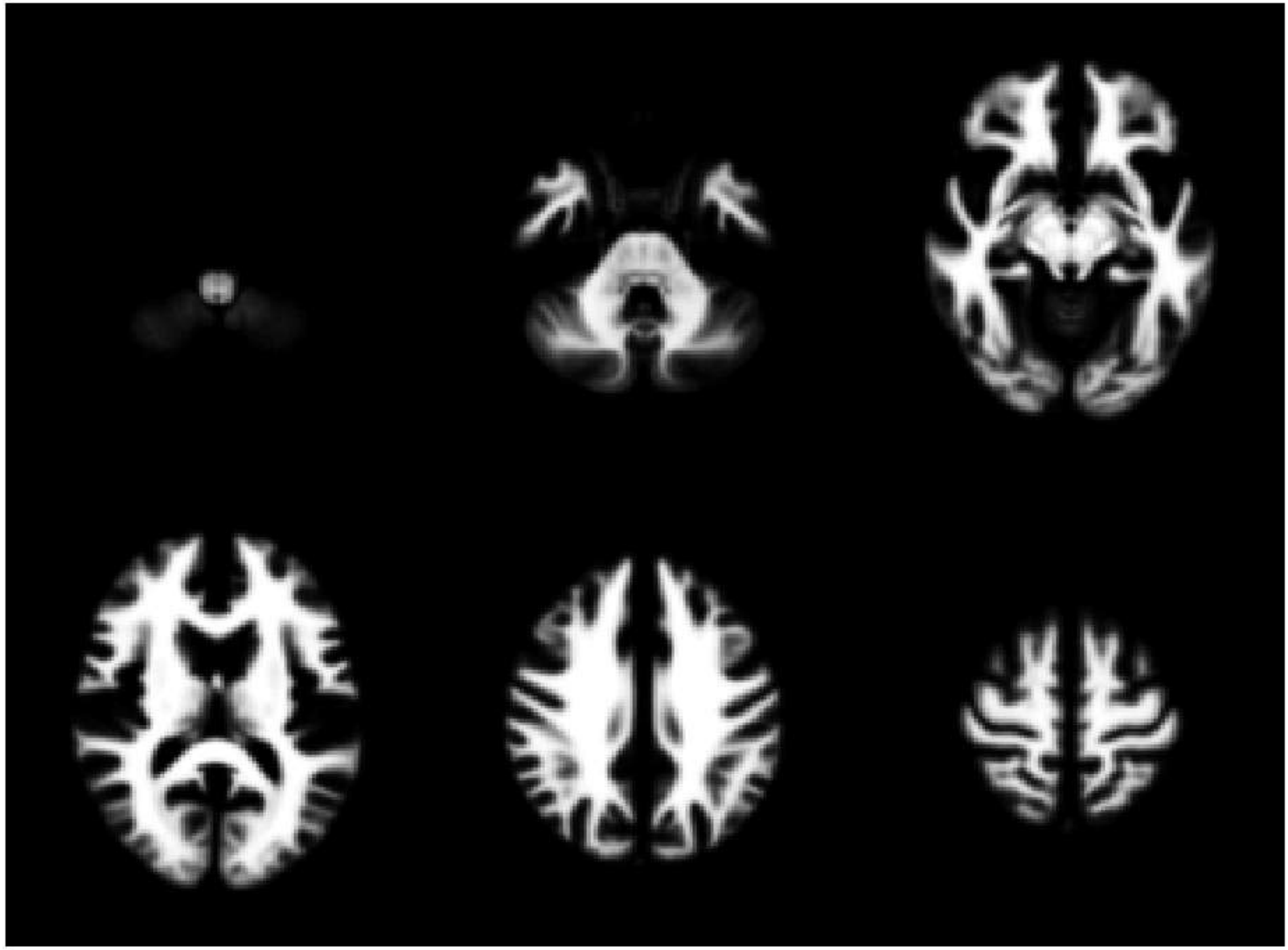
Initial
GM images

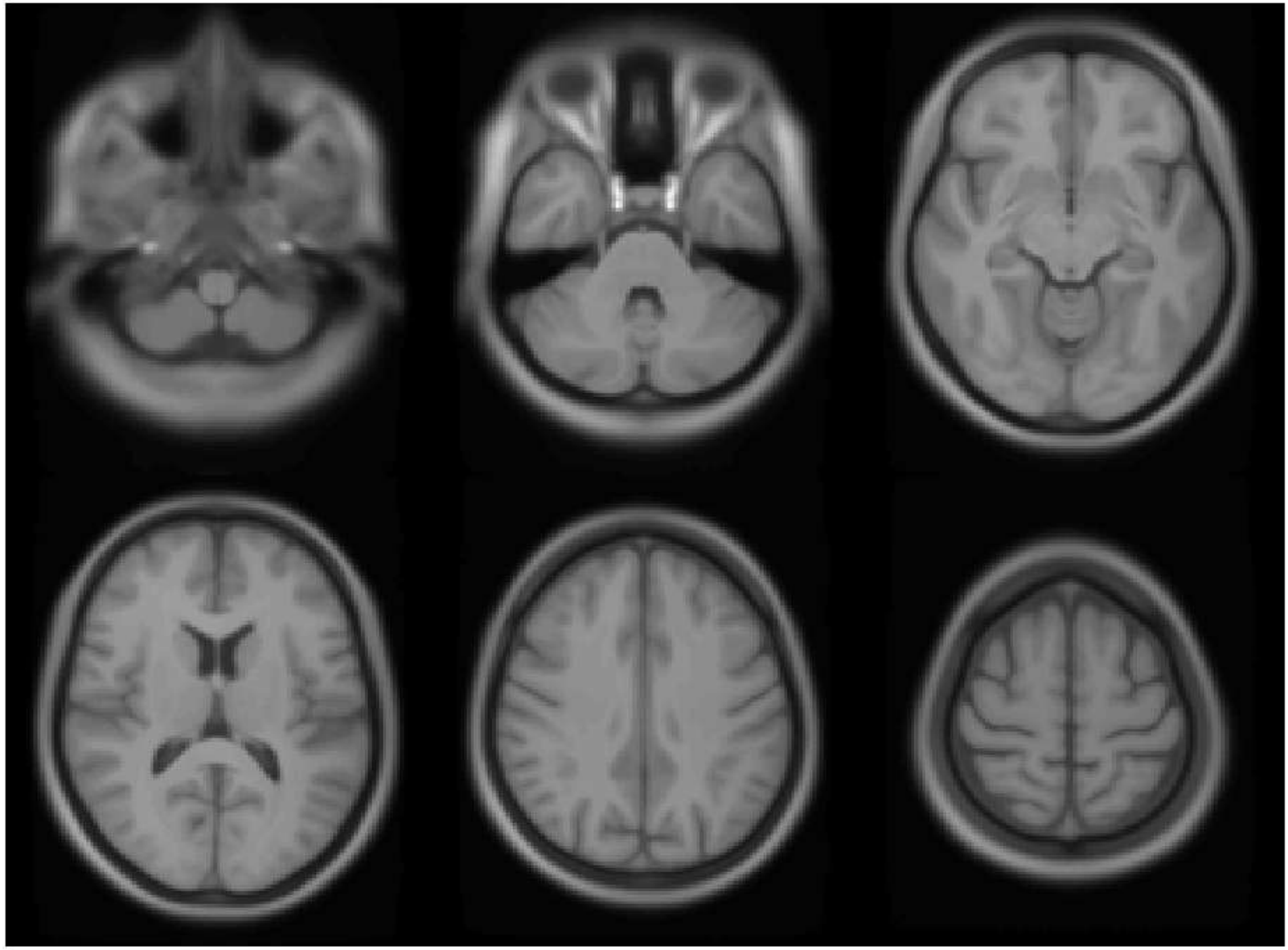


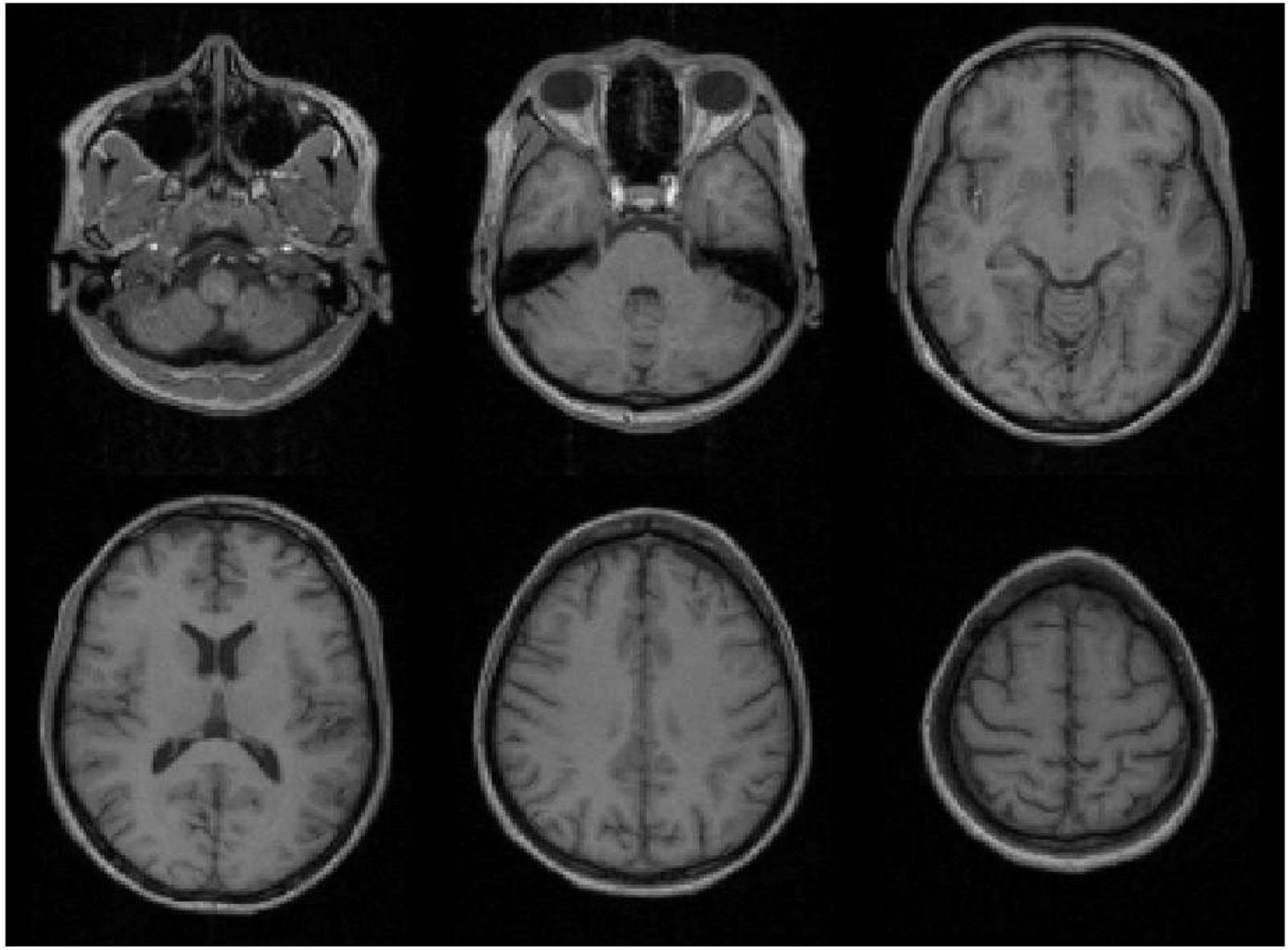
Warped
GM images

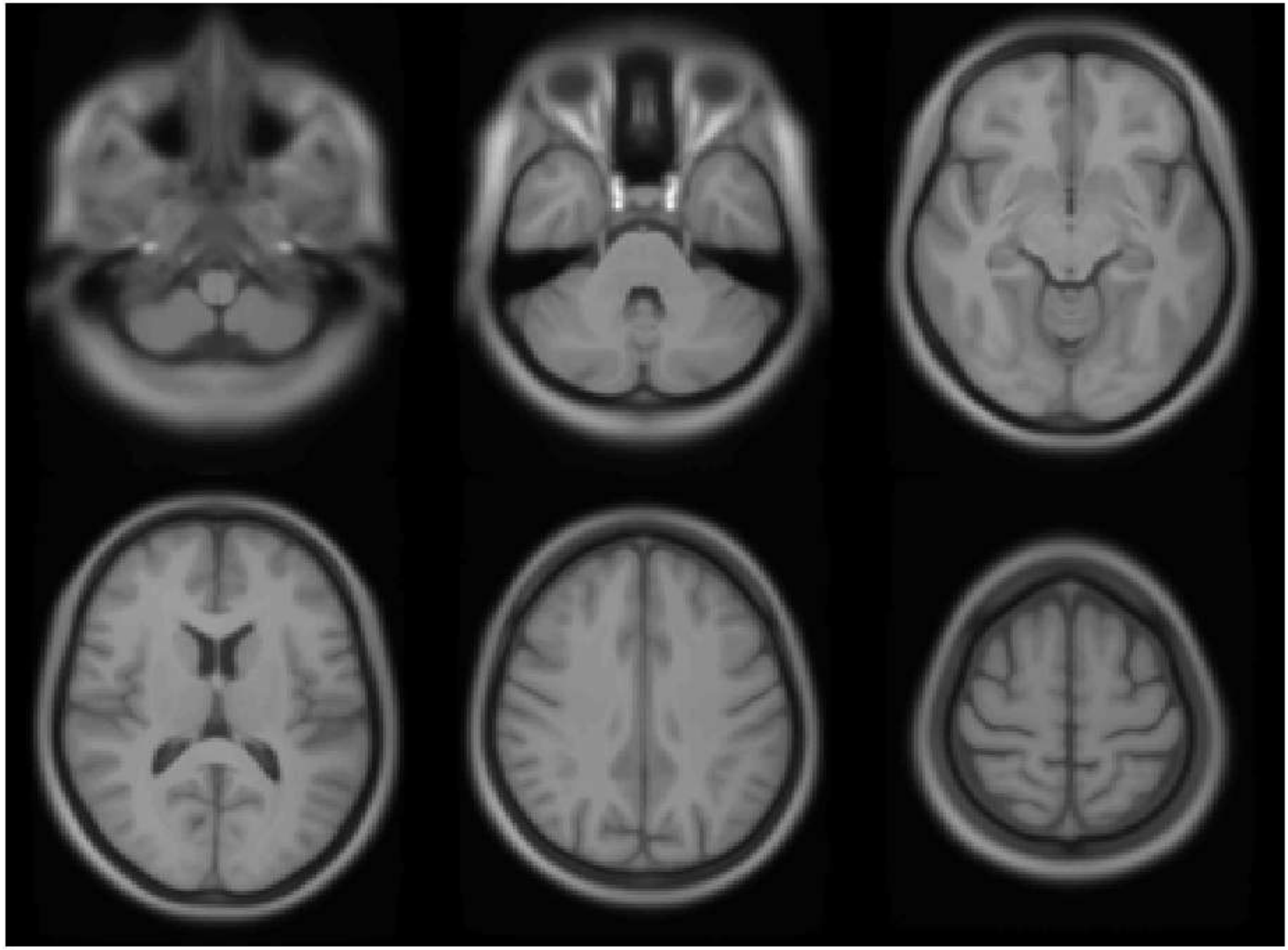


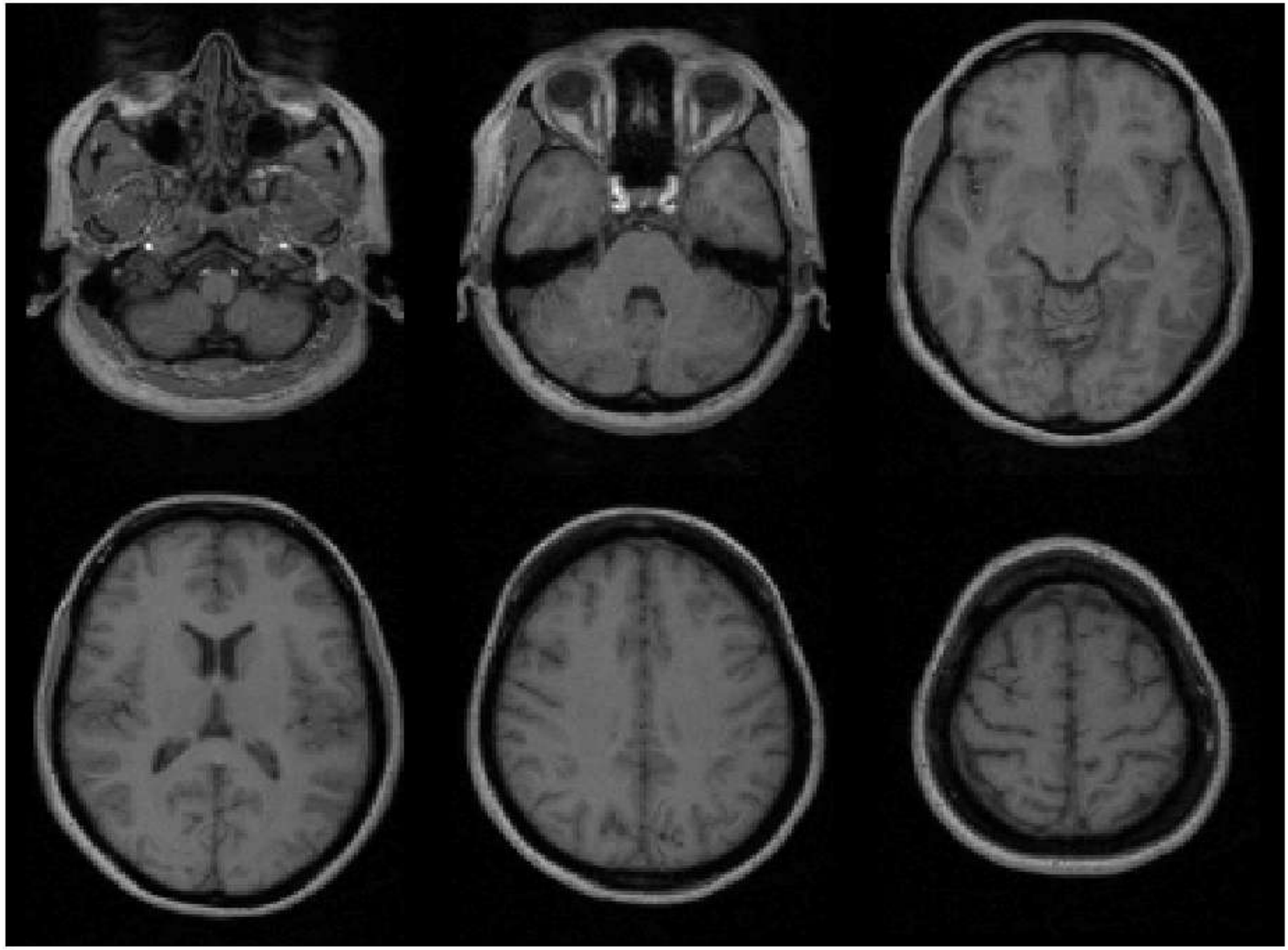


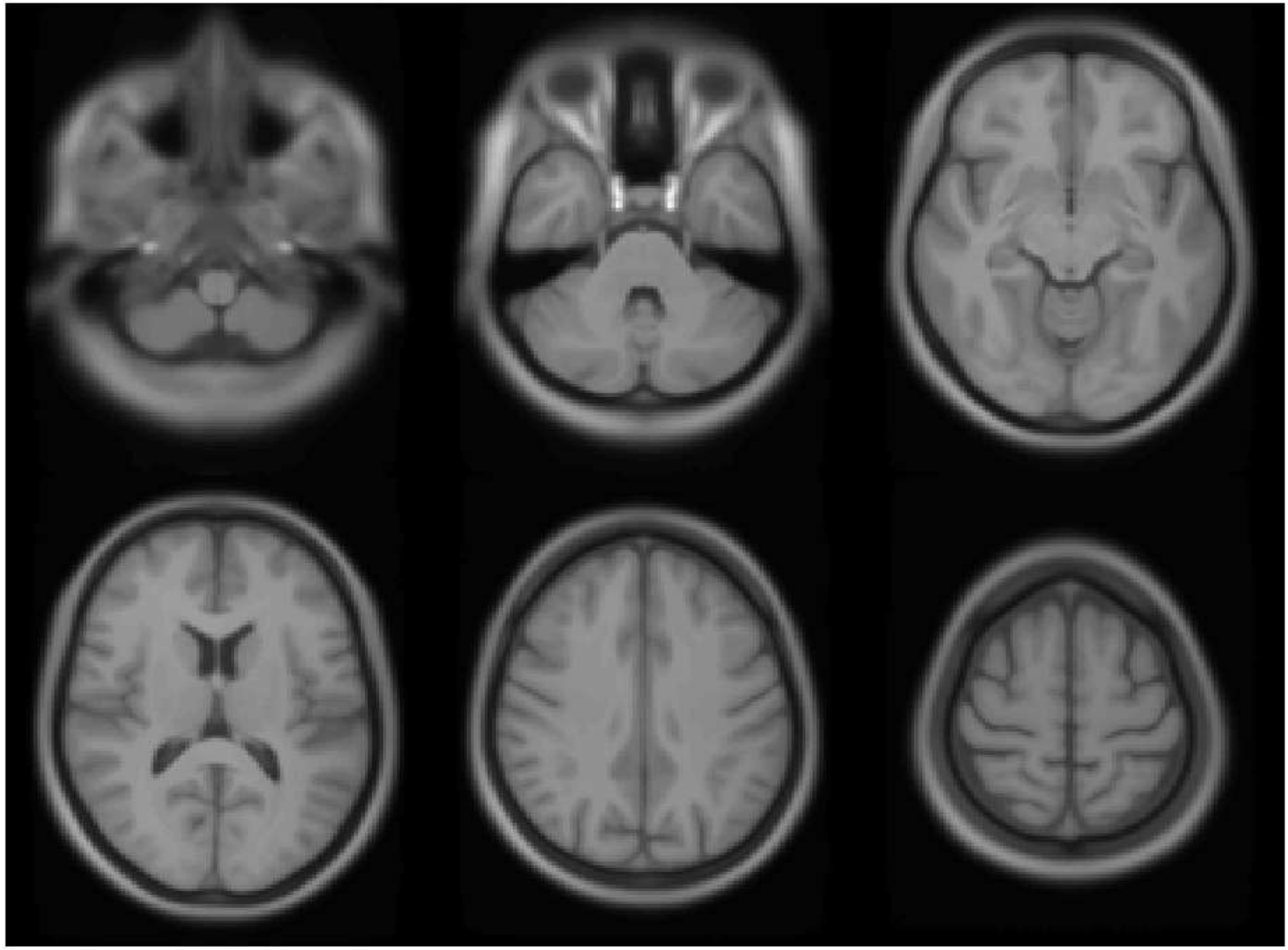


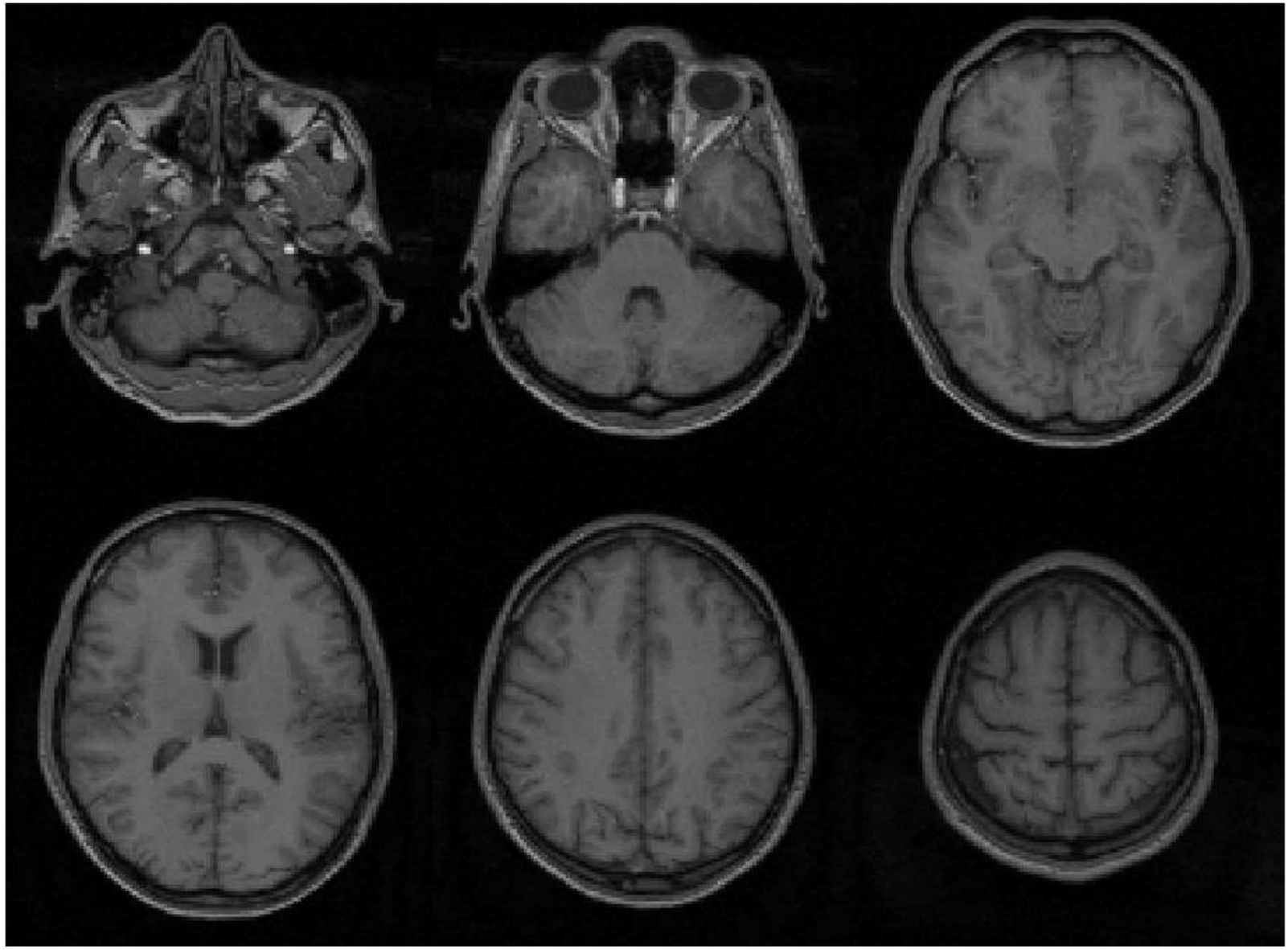


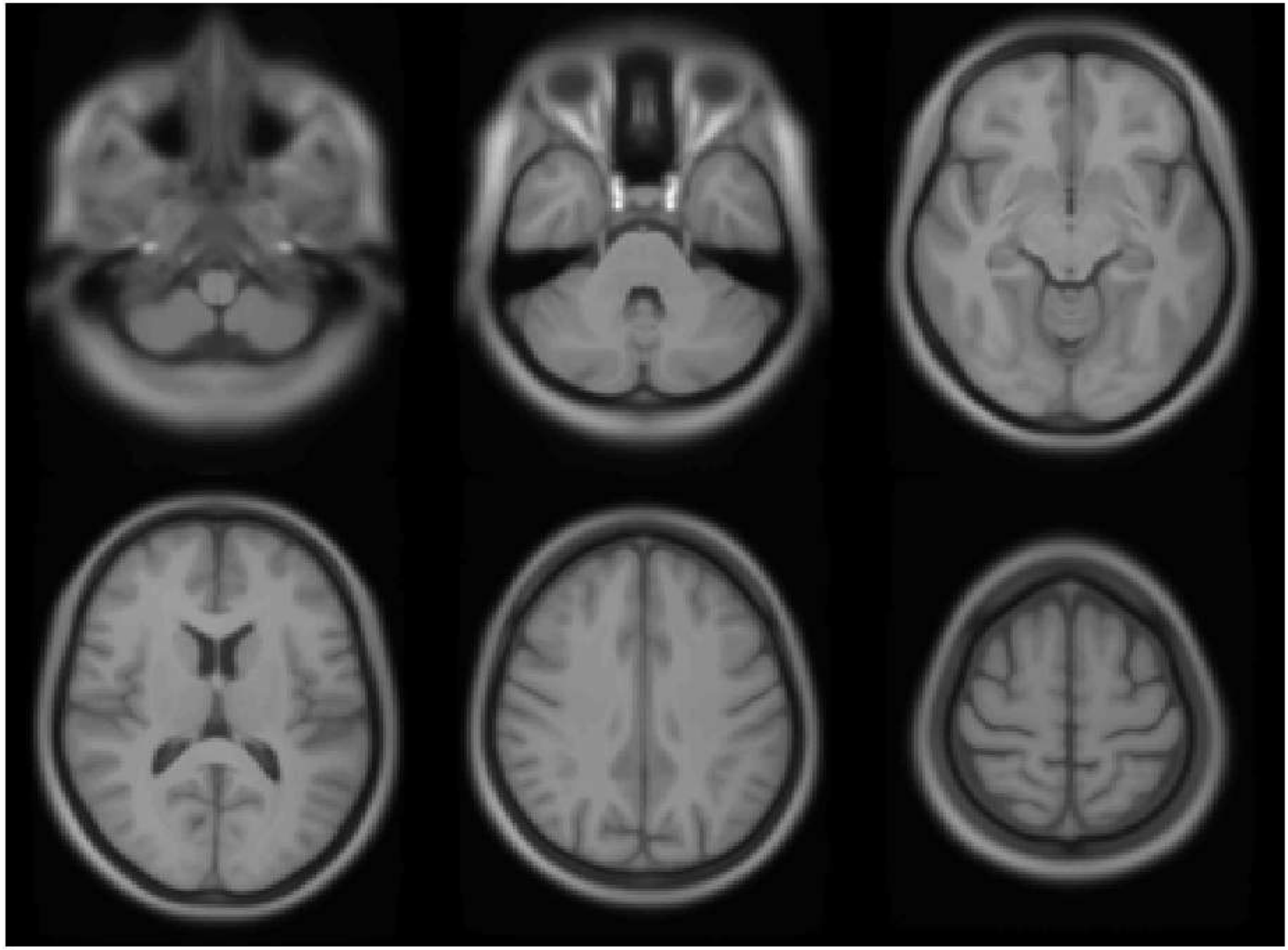


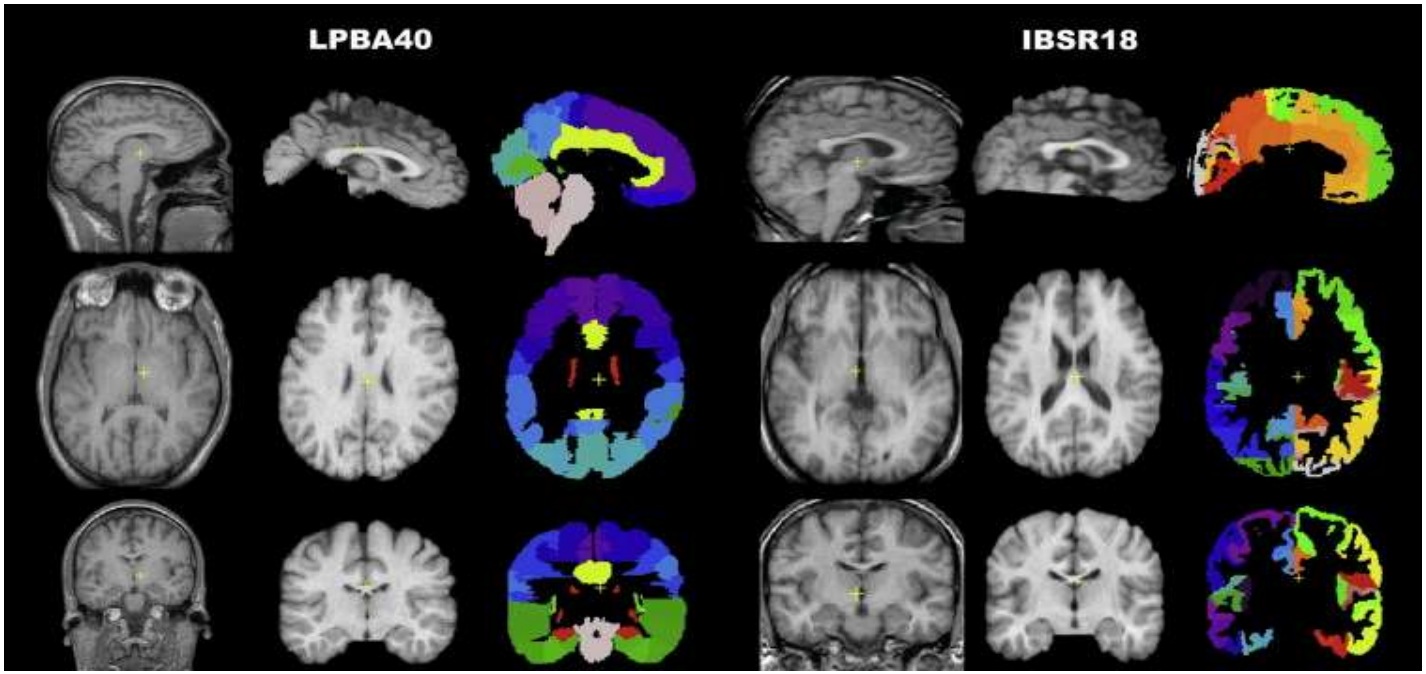




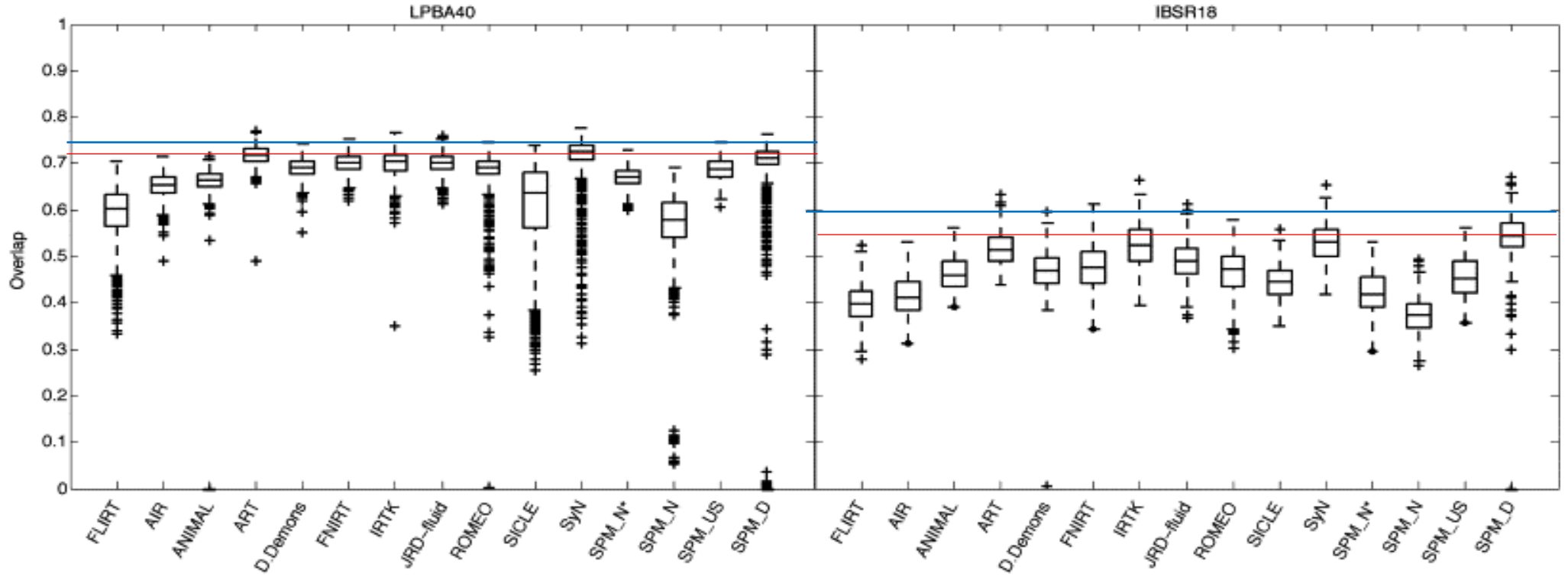


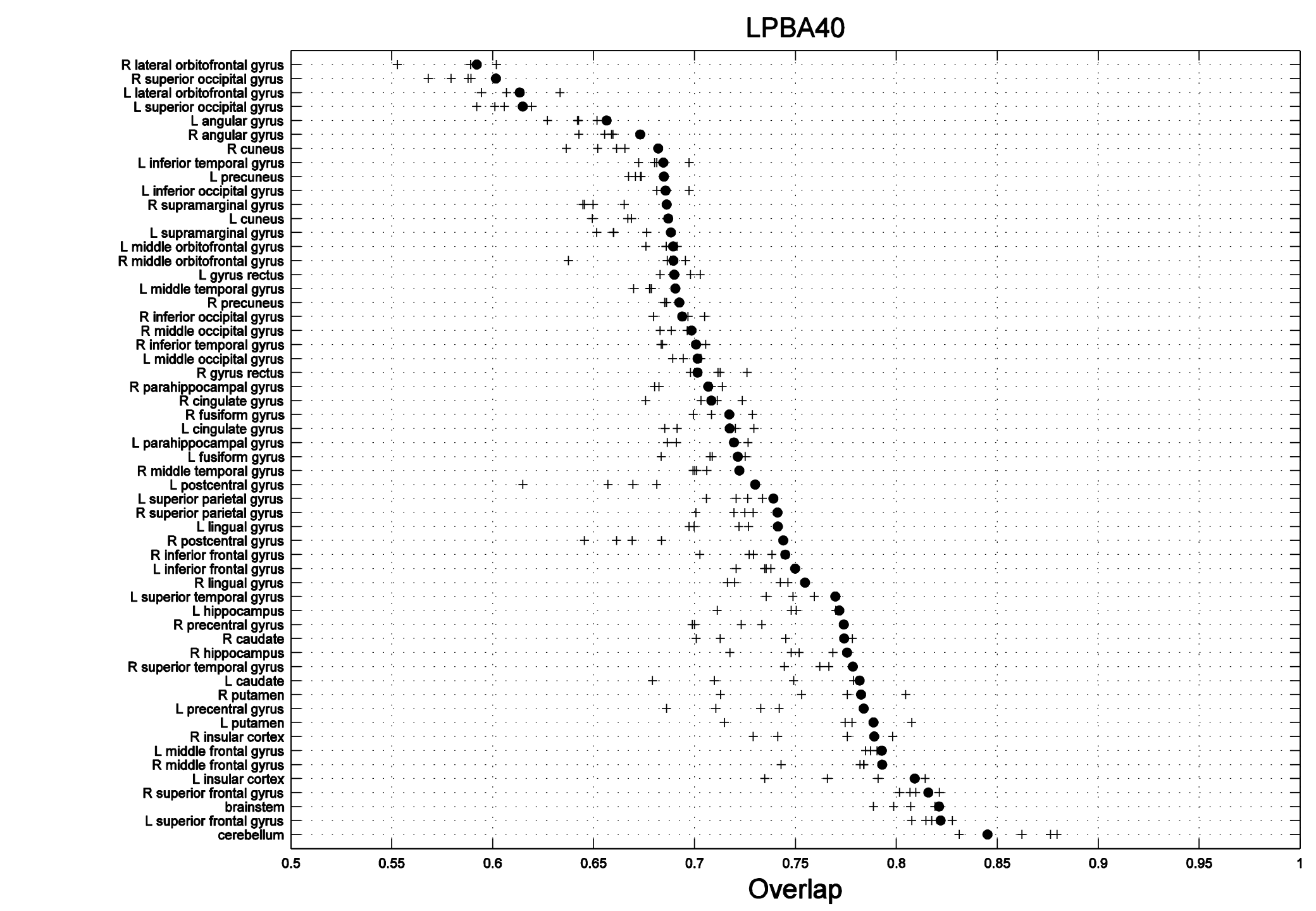






Evaluations of nonlinear registration algorithms




LPBA40
R lateral orbitofrontal gyrus
R superior occipital gyrus
L lateral orbitofrontal gyrus
L superior occipital gyrus
L angular gyrus
R angular gyrus
R cuneus
L inferior temporal gyrus
L precuneus
L inferior occipital gyrus
R supramarginal gyrus
L cuneus
L supramarginal gyrus
L middle orbitofrontal gyrus
R middle orbitofrontal gyrus
L gyrus rectus
L middle temporal gyrus
R precuneus
R inferior occipital gyrus
R middle occipital gyrus
R inferior temporal gyrus
L middle occipital gyrus
R gyrus rectus
R parahippocampal gyrus
R cingulate gyrus
R fusiform gyrus
L cingulate gyrus
L parahippocampal gyrus
L fusiform gyrus
R middle temporal gyrus
L postcentral gyrus
L superior parietal gyrus
R superior parietal gyrus
L lingual gyrus
R postcentral gyrus
R inferior frontal gyrus
L inferior frontal gyrus
R lingual gyrus
L superior temporal gyrus
L hippocampus
R precentral gyrus
R caudate
R hippocampus
R superior temporal gyrus
L caudate
R putamen
L precentral gyrus
L putamen
R insular cortex
L middle frontal gyrus
R middle frontal gyrus
L insular cortex
R superior frontal gyrus
brainstem
L superior frontal gyrus
cerebellum
0.5
0.55
0.6
0.65
0.7
0.75
0.8
0.85
0.9
0.95
1
Overlap

Why use diffeomorphic registration?

$$2 \times 2 \neq 3$$

This is what you get from approximating a multiplication using additions.

$$((2-1)+(2-1))+1 = 3$$

It almost works for values close to 1.

$$1.01 \times 1.01 = 1.0201$$

$$((1.01-1)+(1.01-1))+1 = 1.02$$

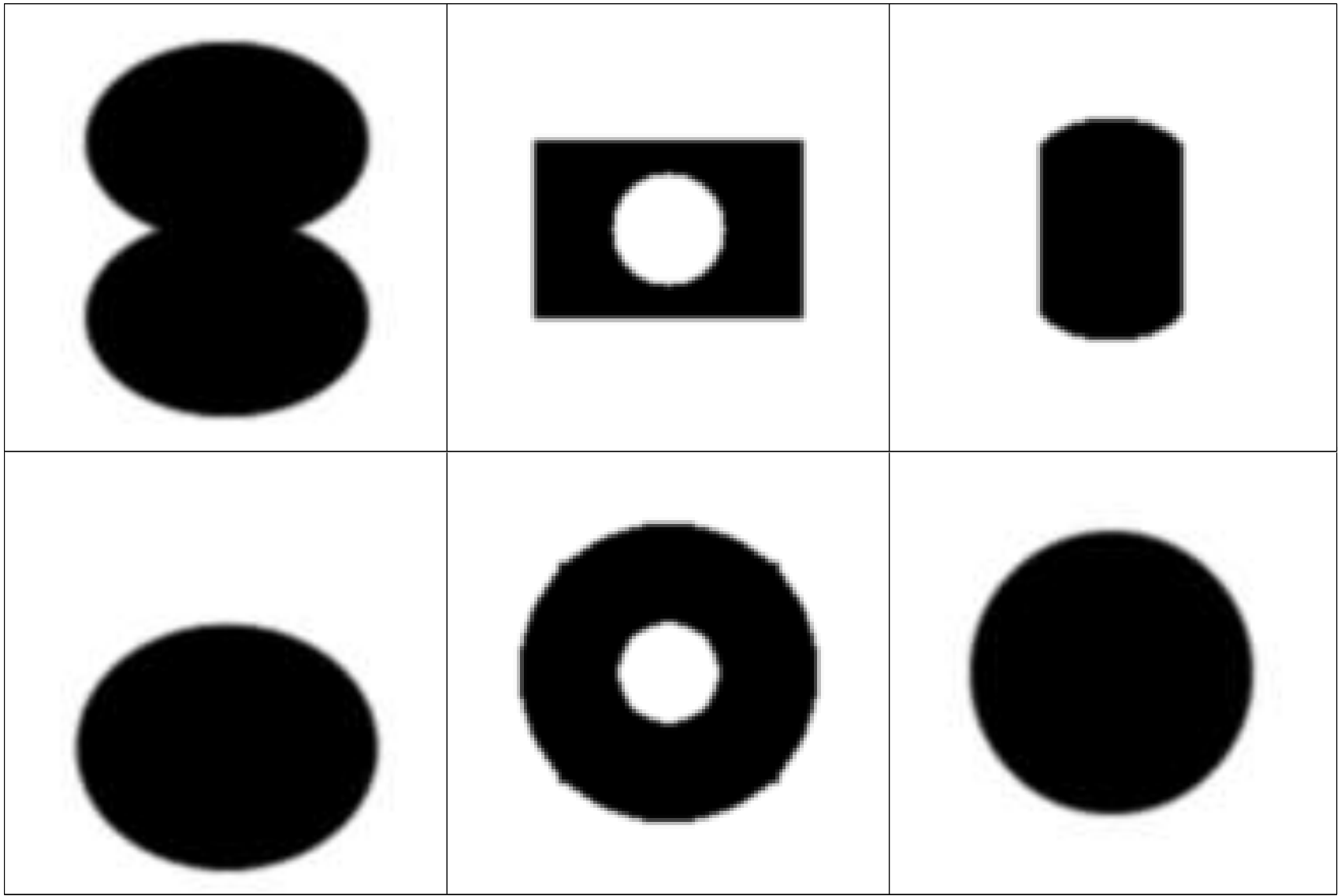
Some References

- Ashburner. "*A Fast Diffeomorphic Image Registration Algorithm*". NeuroImage 38:95-113, 2007.
- Ashburner & Friston. "*Computing Average Shaped Tissue Probability Templates*". NeuroImage **45**:333-341, 2009.
- Ashburner & Friston. "*Diffeomorphic registration using geodesic shooting and Gauss–Newton optimisation*". NeuroImage 55(3):954-967, 2011.
- Klein, Andersson, Ardekani, Ashburner, Avants, Chiang, Christensen, Collins, Gee, Hellier, Song, Jenkinson, Lepage, Rueckert, Thompson, Vercauteren, Woods, Mann & Parsey. "*Evaluation of 14 nonlinear deformation algorithms applied to human brain MRI registration*". NeuroImage 46:786-802, 2009.

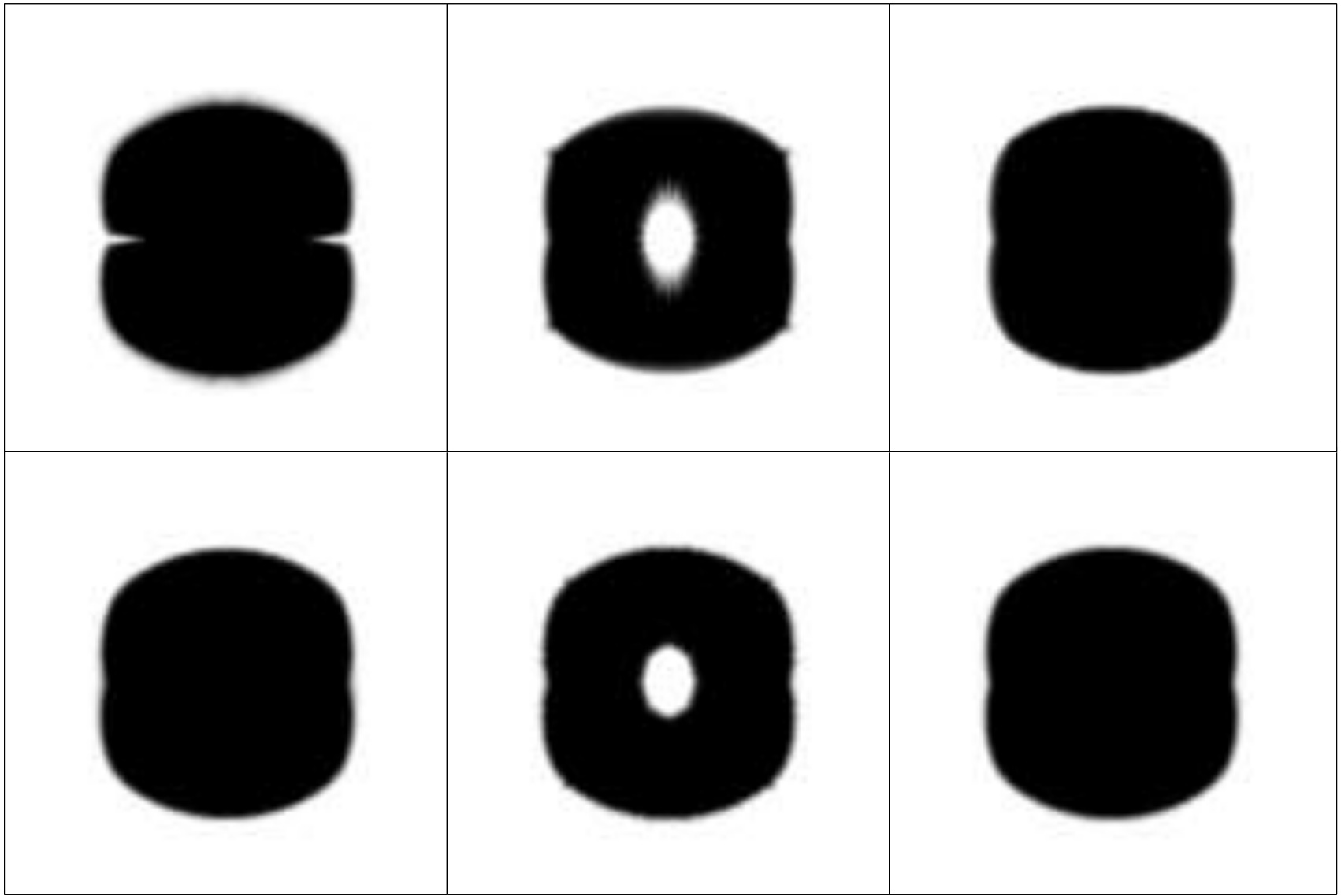
Overview

- Voxel-Based Morphometry
- Diffeomorphic Registration
- **Tensor-Based Morphometry**
- Longitudinal Registration

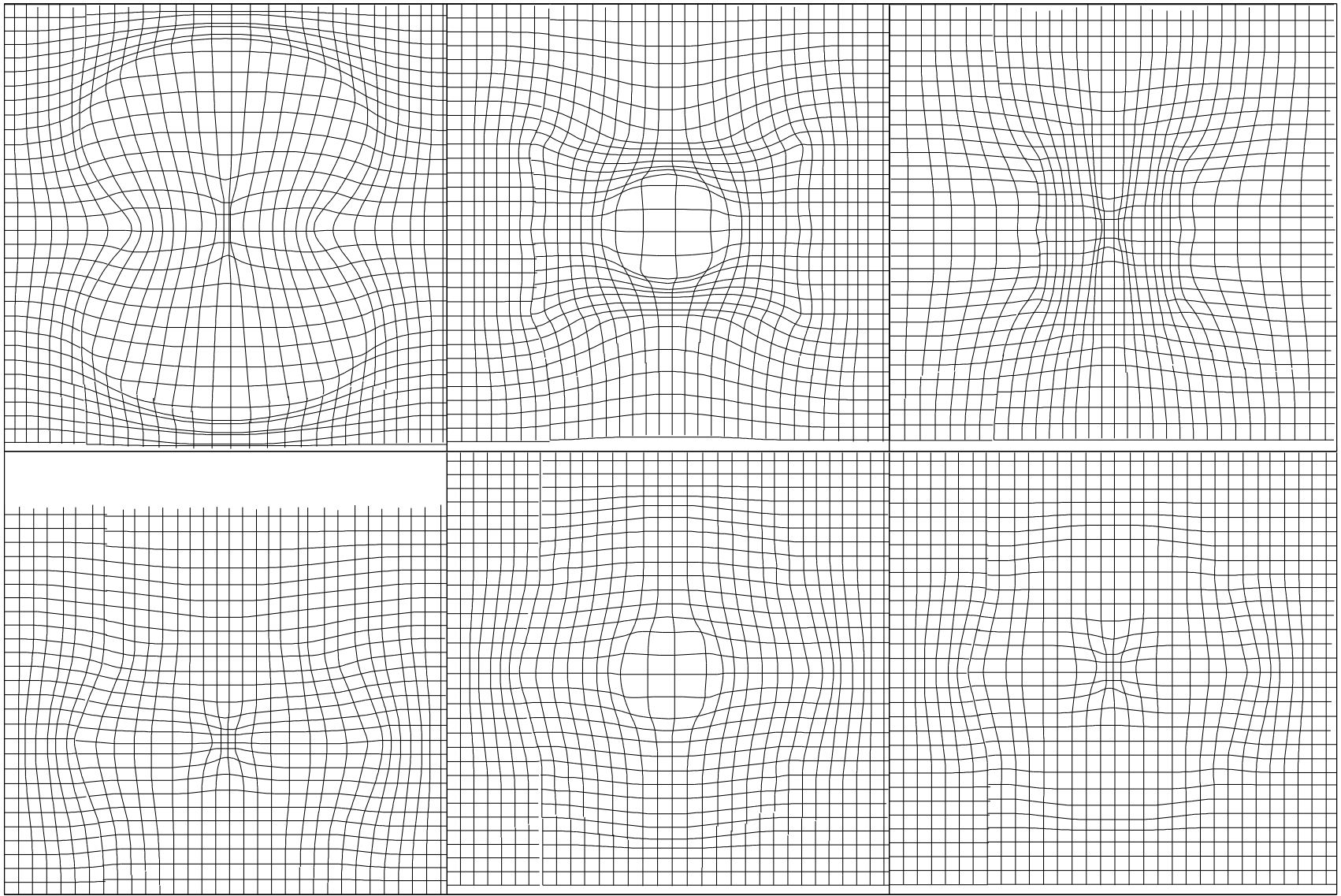
Some 2D Shapes



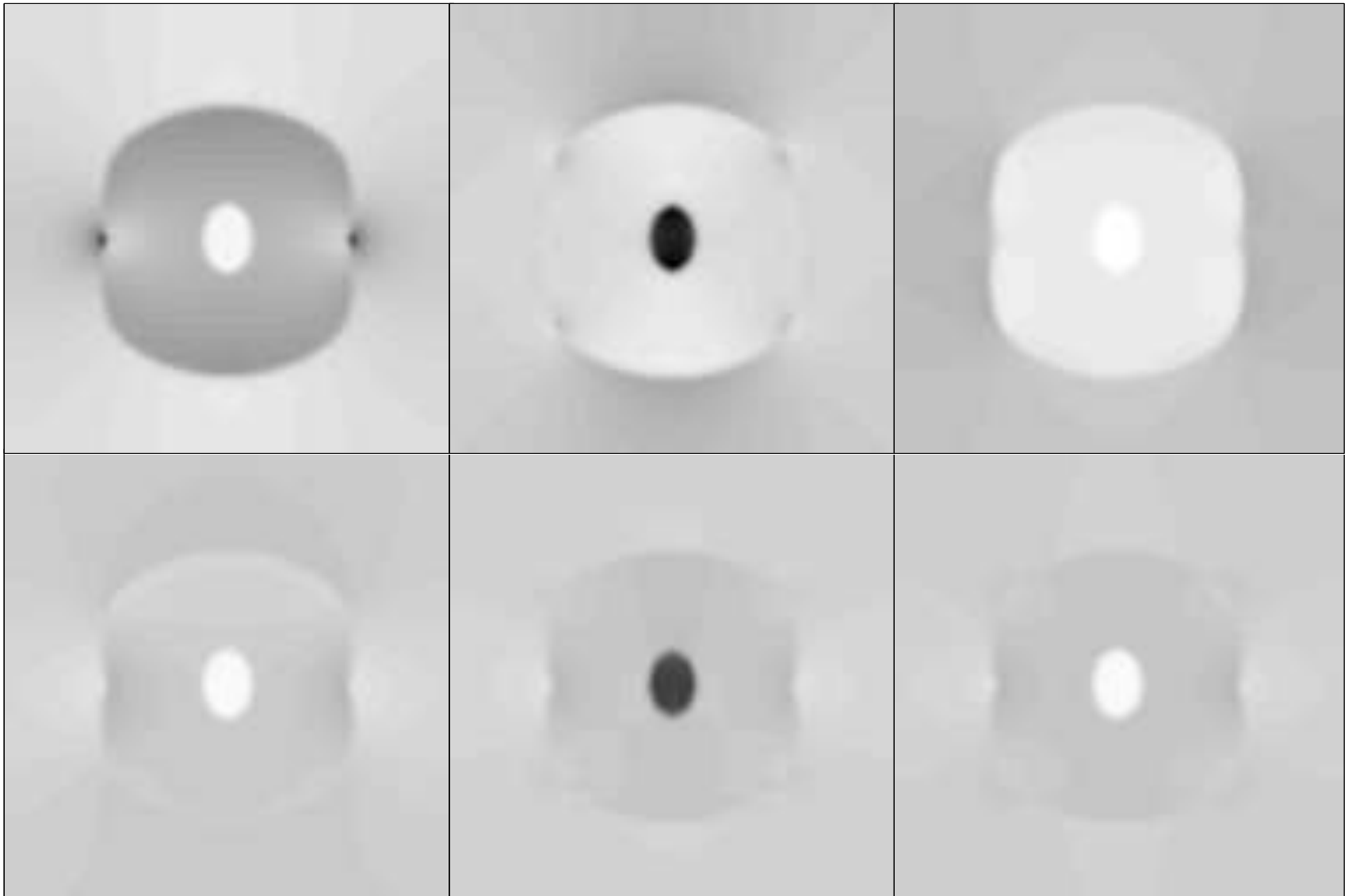
Shapes aligned to their average



These were the deformations for that



and these are the Jacobian determinants



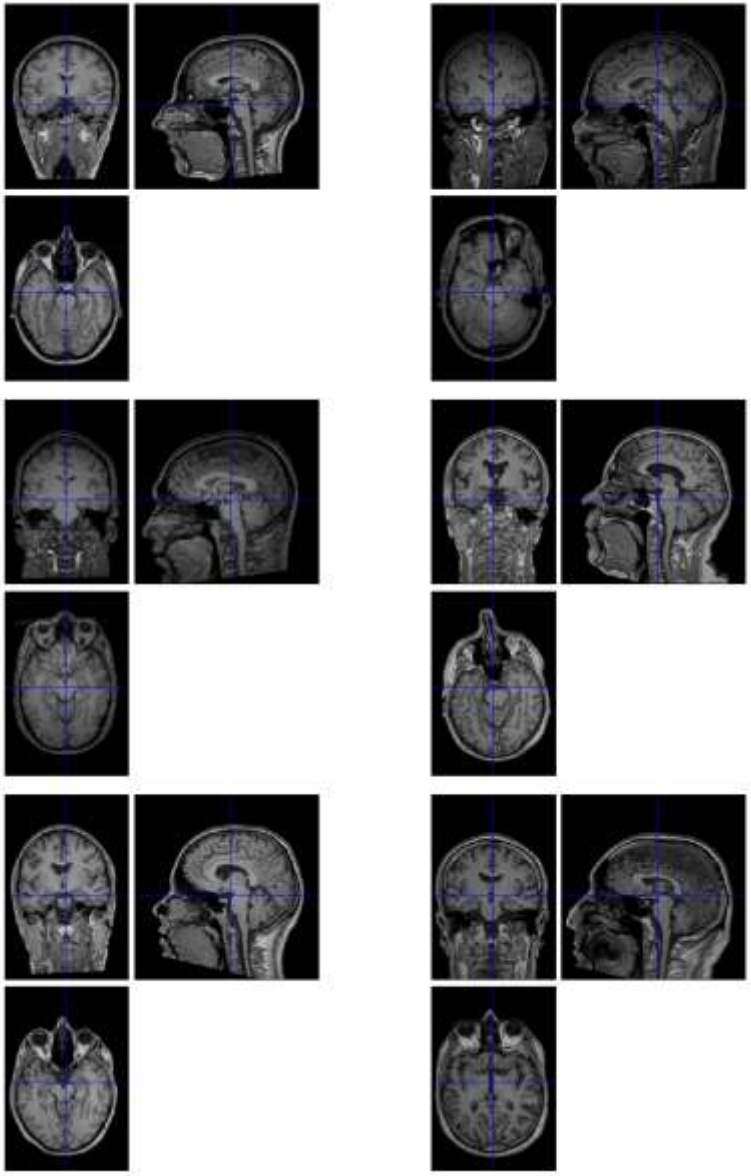
Cross-Sectional Data

Used 550 T1w brain MRI from IXI (Information eXtraction from Images) dataset.

- http://www.brain-development.org/

Data from three different hospitals in London:

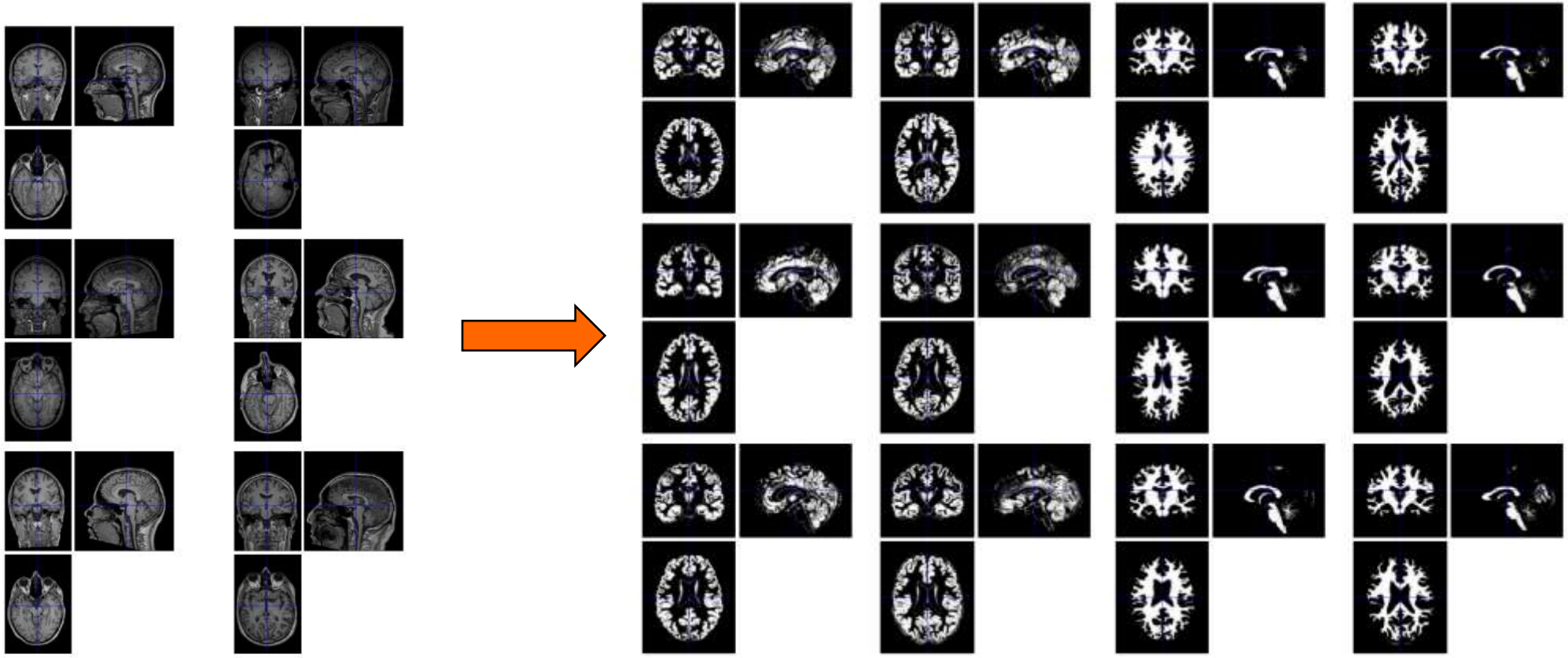
- Hammersmith Hospital using a Philips 3T system
- Guy's Hospital using a Philips 1.5T system
- Institute of Psychiatry using a GE 1.5T system5T system



Segmentation

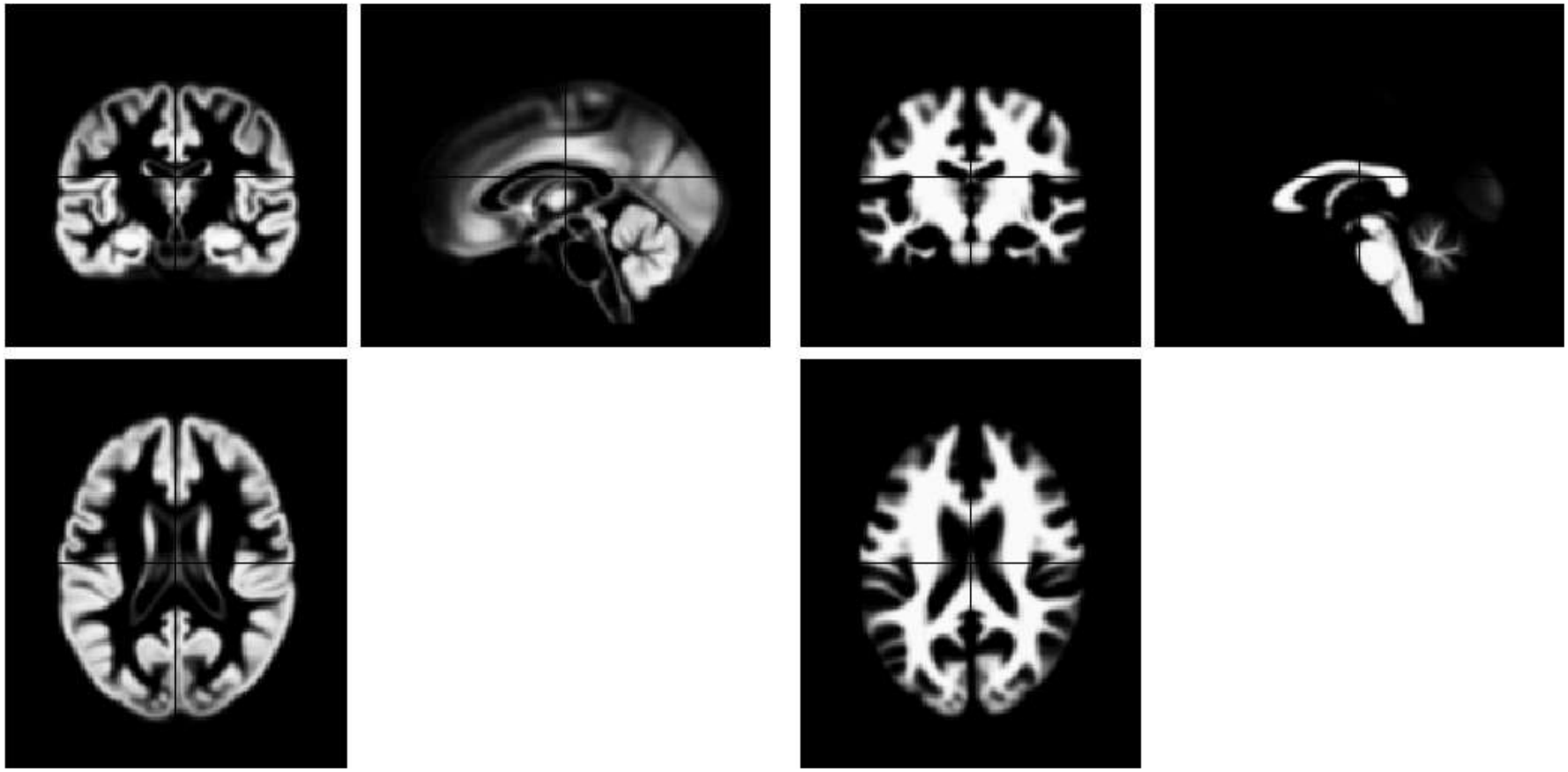
Segmented into GM and WM.

Approximately aligned via rigid-body.



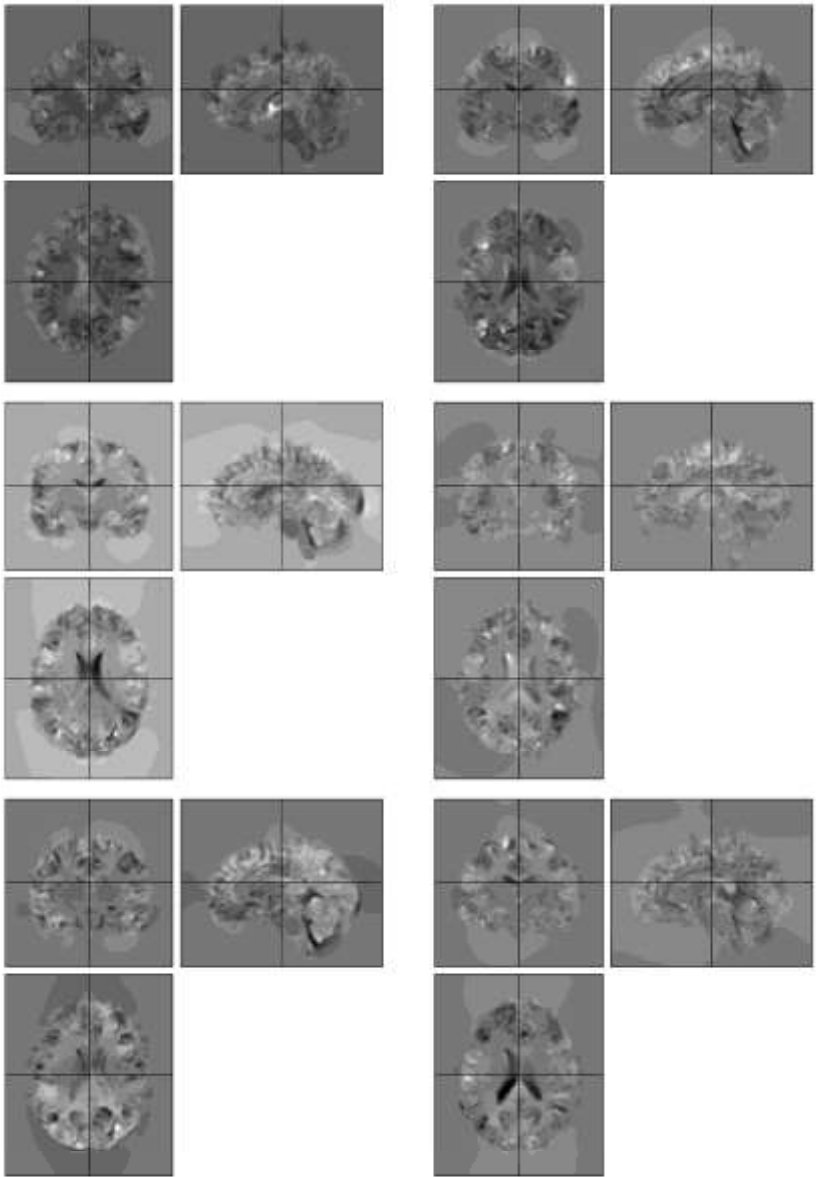
Diffeomorphic Alignment

All GM and WM were diffeomorphically aligned to their common average-shaped template.

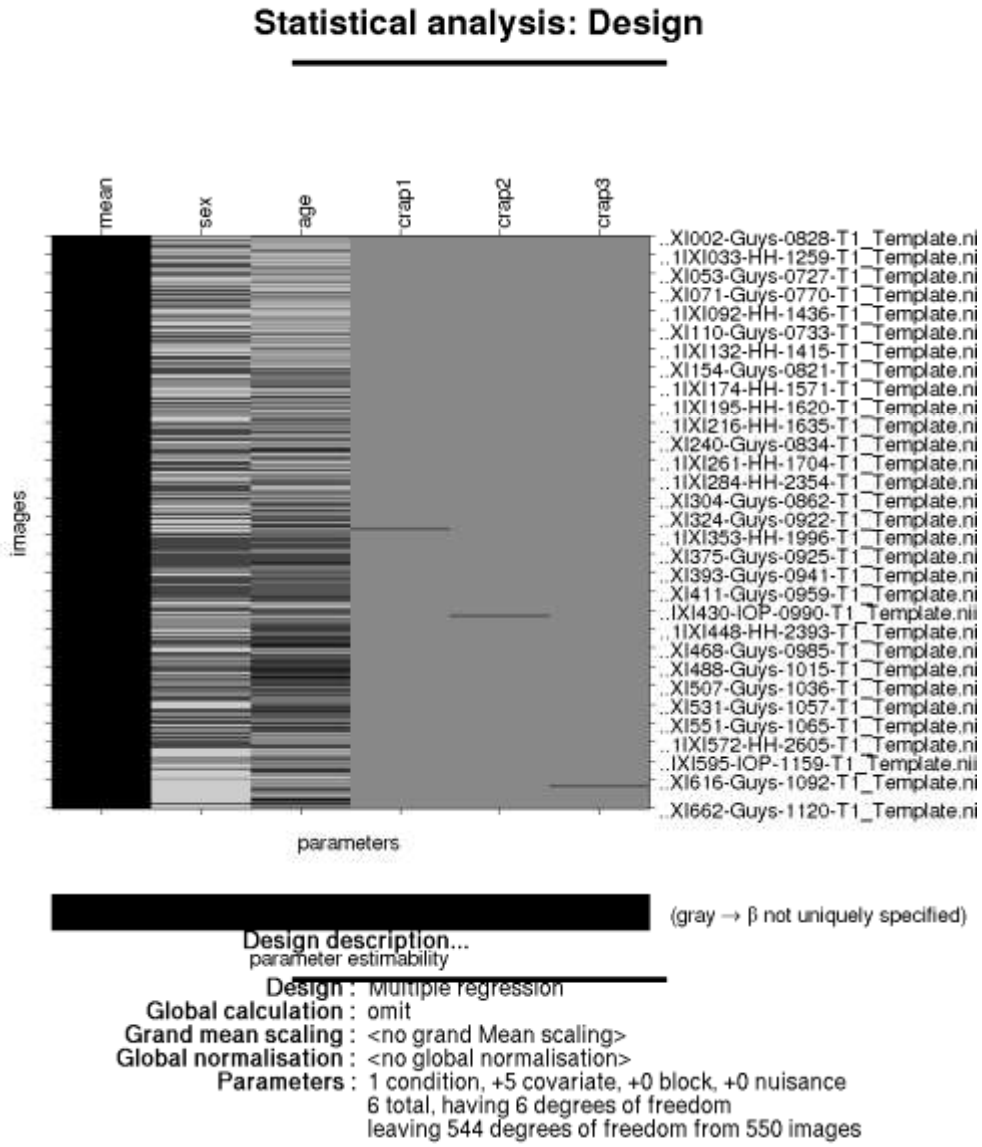


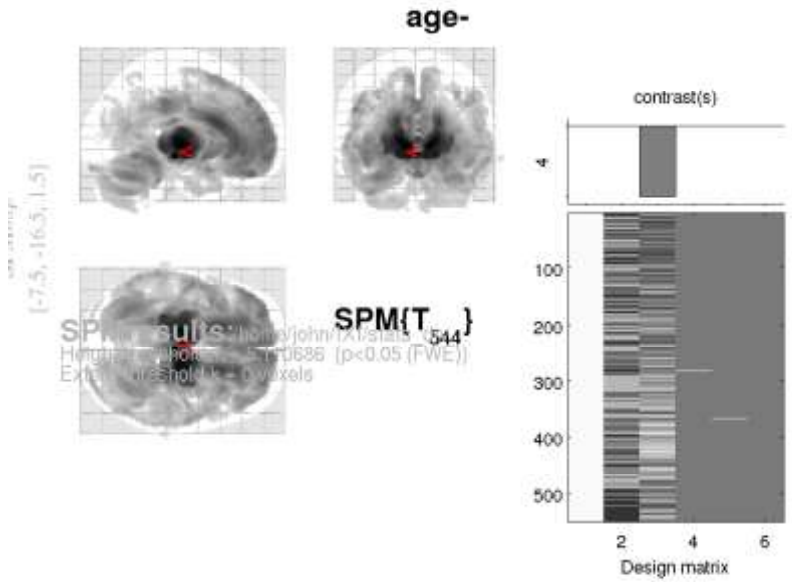
Divergence Maps

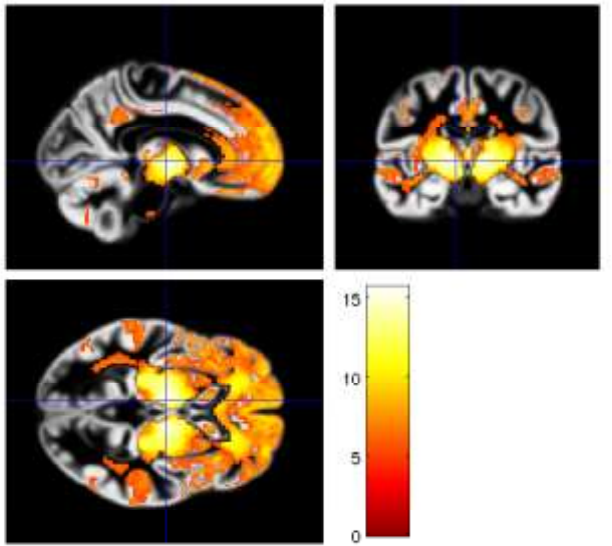
- Used maps of initial velocity divergence.
- Similar to logarithms of Jacobian determinants.
  - Encode a sort of “growth rate”



Mass-Univariate Analysis – shrinkage with age

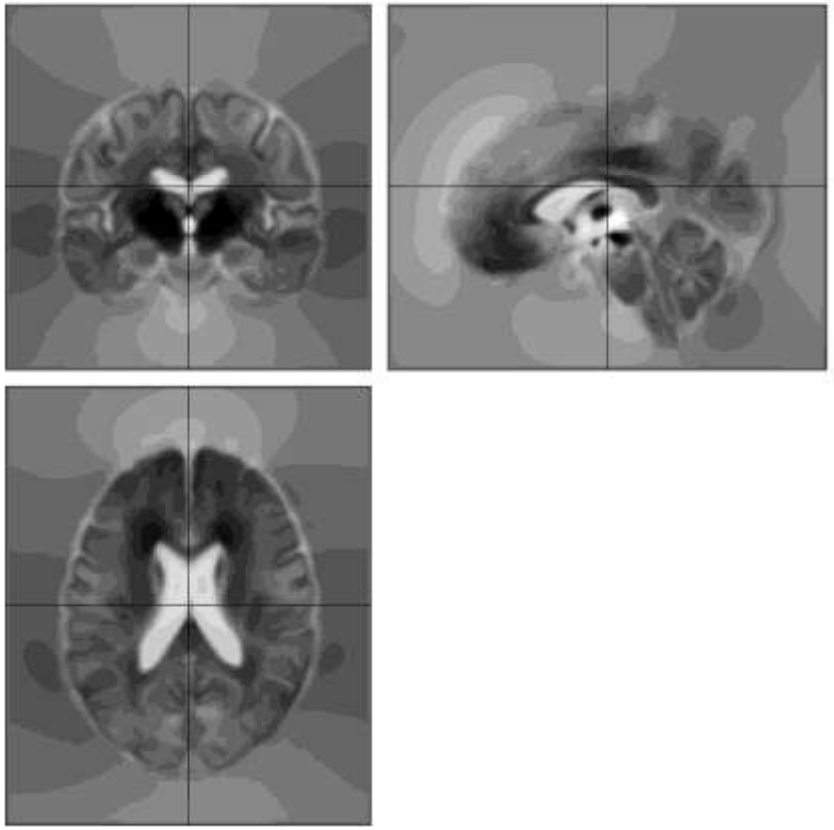




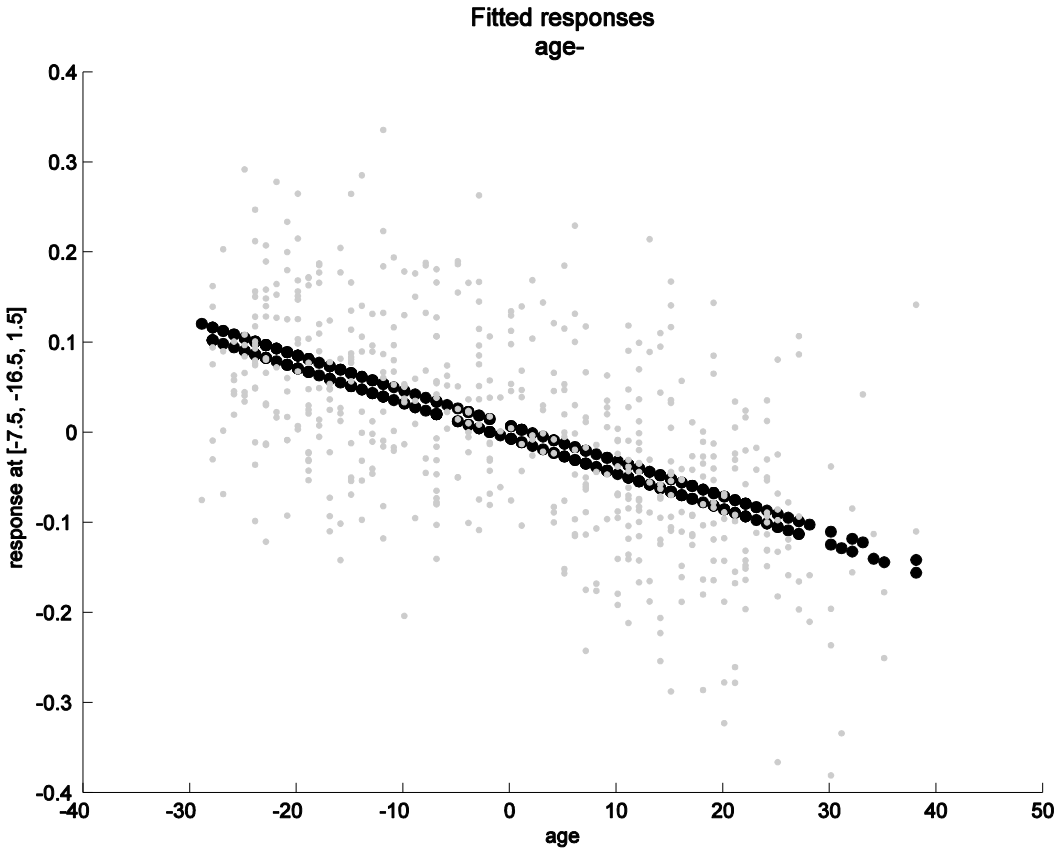


Large T statistics (> 15) – but not very predictive

T Statistic Image



The most predictive single voxel



Some References

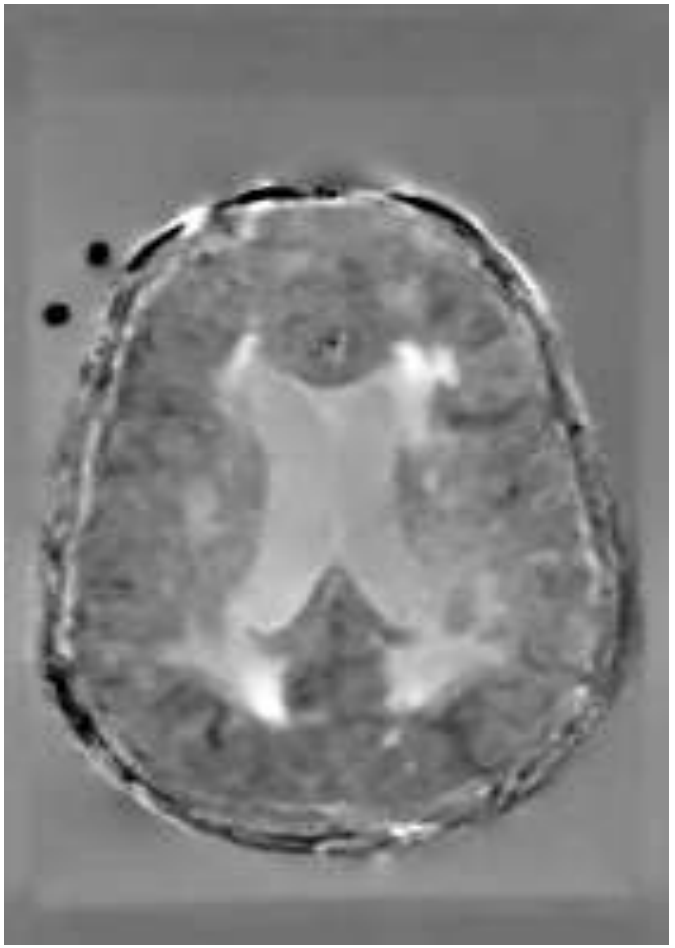
- Ashburner & Friston. "*Unified Segmentation*". NeuroImage **26**:839-851, 2005.
- Ashburner & Friston. "*Computing Average Shaped Tissue Probability Templates"*. NeuroImage **45**:333-341, 2009.
- Ashburner & Friston. "*Diffeomorphic registration using geodesic shooting and Gauss–Newton optimisation"*. NeuroImage 55(3):954-967, 2011.

Overview

- Voxel-Based Morphometry
- Diffeomorphic Registration
- Tensor-Based Morphometry
- **Longitudinal Registration**

Longitudinal Registration

- Unified model combines:
  - Nonlinear diffeomorphic registration.
  - Rigid-body registration.
  - Intensity inhomoheneity correction.
- All made as mathematically coherent as possible.

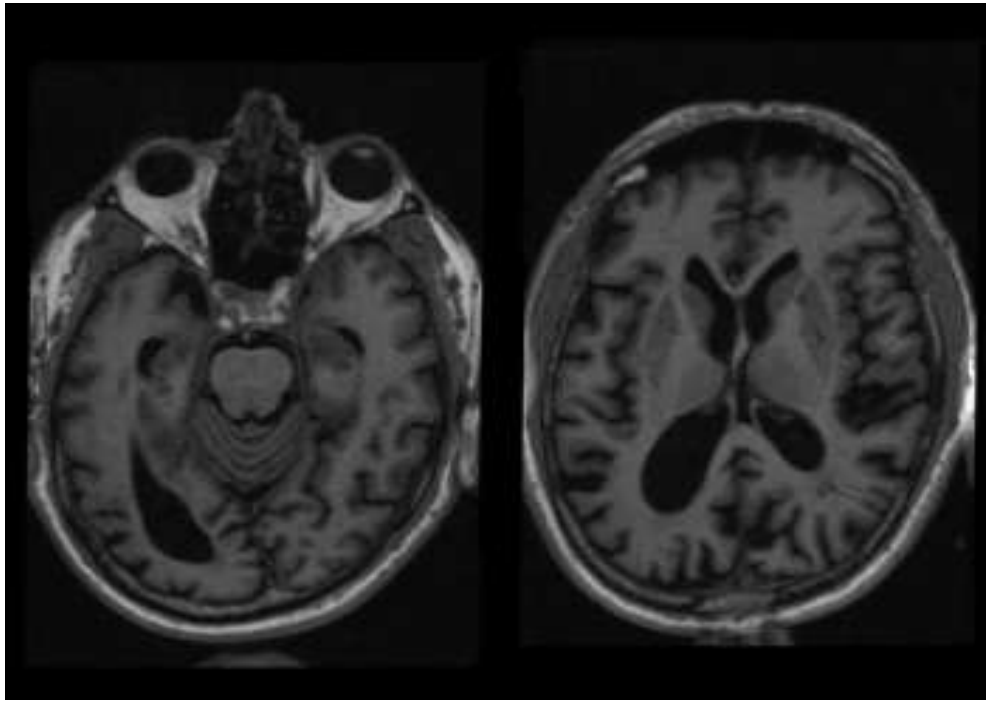


OASIS Data

OAS2 0048

66 year old male with dementia (MMSE=19, CDR=1).

Five scans collected over 40 months.



Marcus, D., A. Fotenos, J. Csernansky, J. Morris, and R. Buckner (2010). *Open access series of imaging studies: longitudinal MRI data in nondemented and demented older adults*. Journal of cognitive neuroscience 22 (12), 2677–2684.

OASIS Data

OAS2 0048

66 year old male with dementia (MMSE=19, CDR=1).

Five scans collected over 40 months.

Difference between time point and first scan.

OASIS Data

OAS2 0048

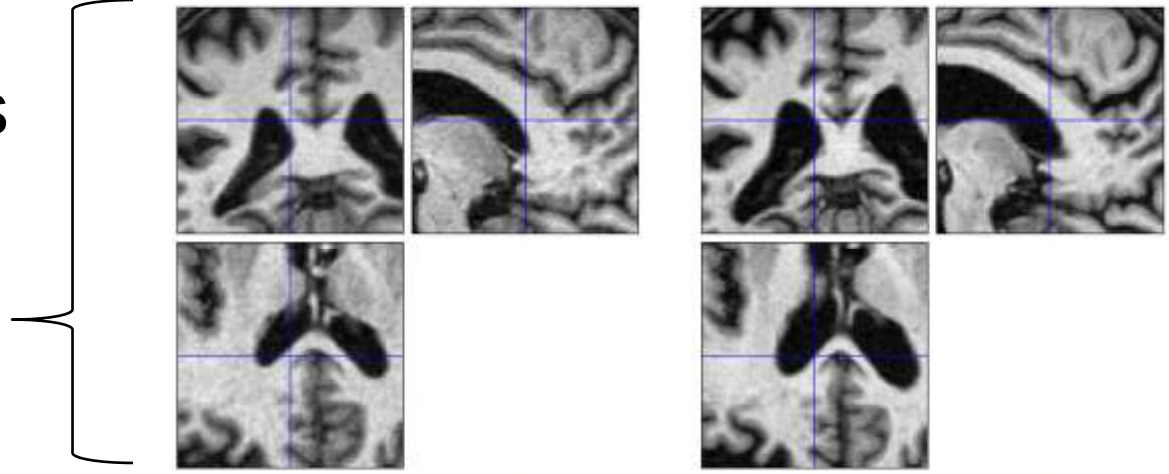
66 year old male with dementia (MMSE=19, CDR=1).

Five scans collected over 40 months.

Expansion/contraction.

Two Longitudinal Scans

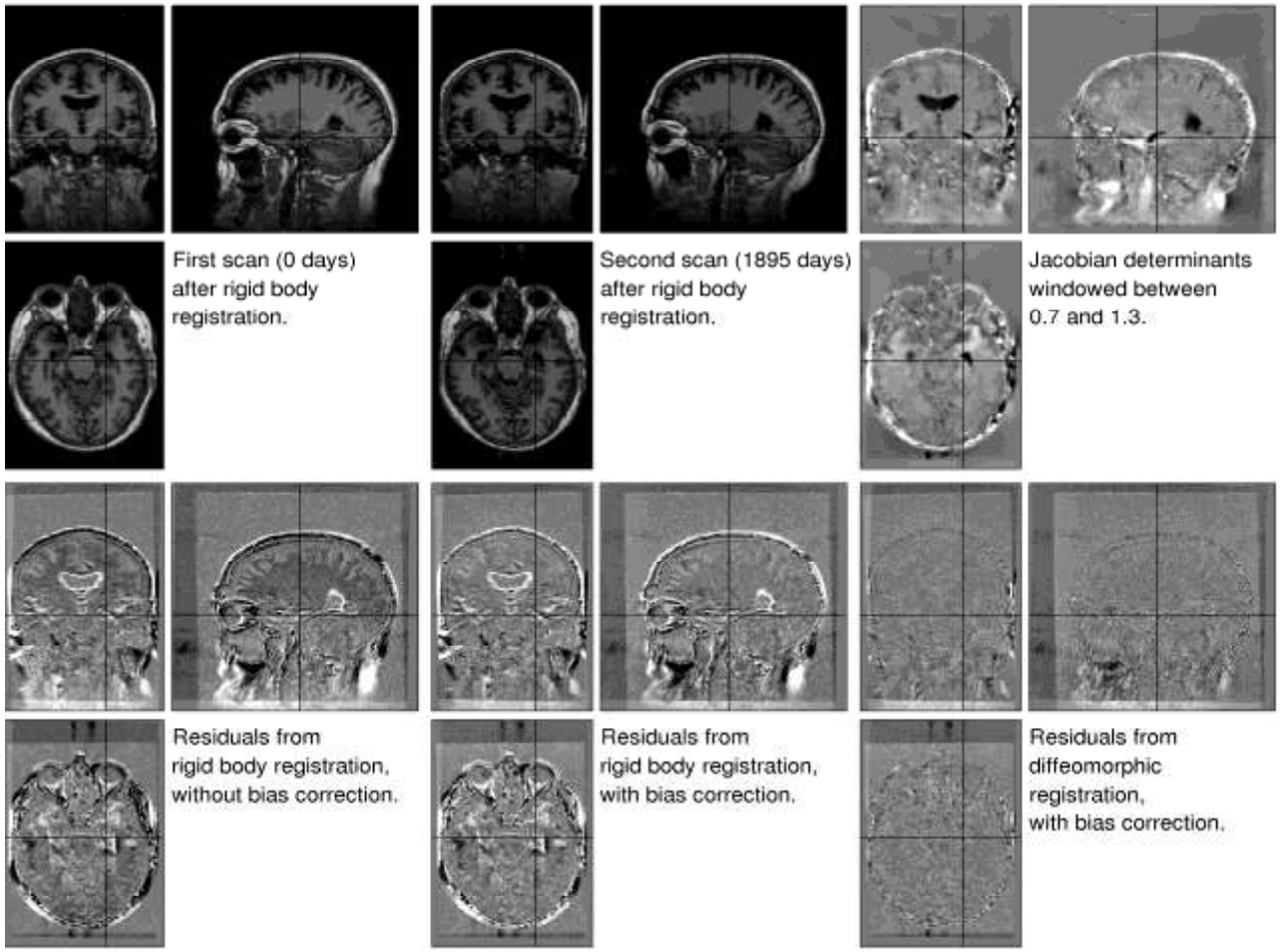
Two scans taken 6 years apart
(after rigid registration).



Oasis Data

OAS2 0002

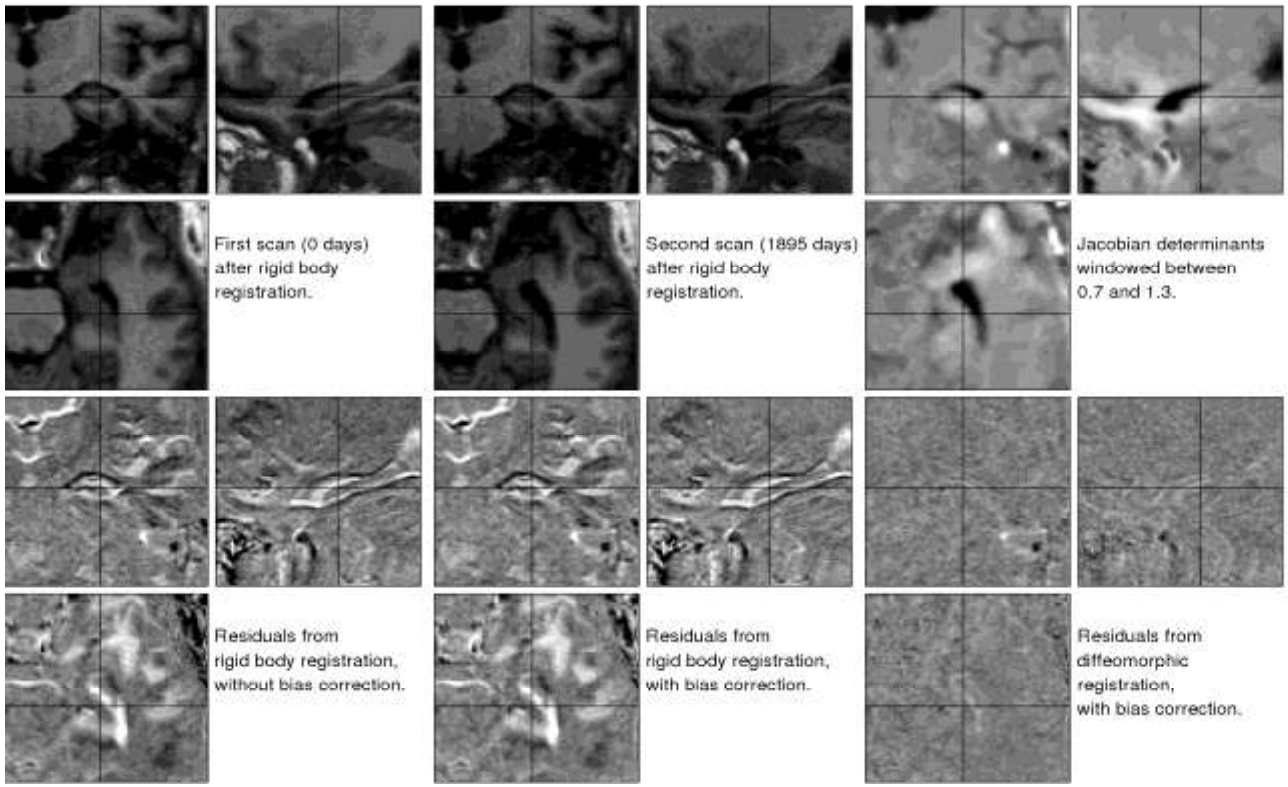
75 year old male, with MCI (MMSE=22, CDR=0.5).



Oasis Data

OAS2 0002

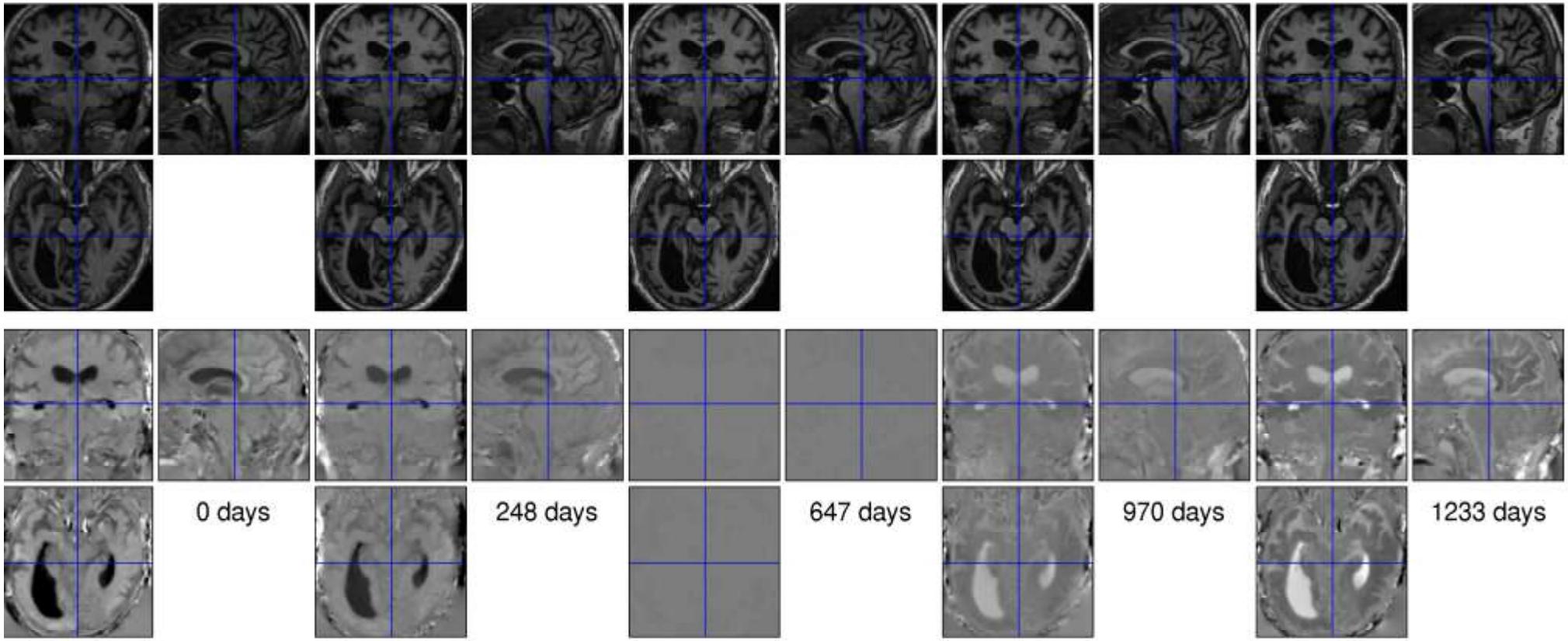
75 year old male, with MCI (MMSE=22, CDR=0.5).



Oasis Data

OAS2 0048

66 year old male, with MCI (MMSE=19, CDR=1).



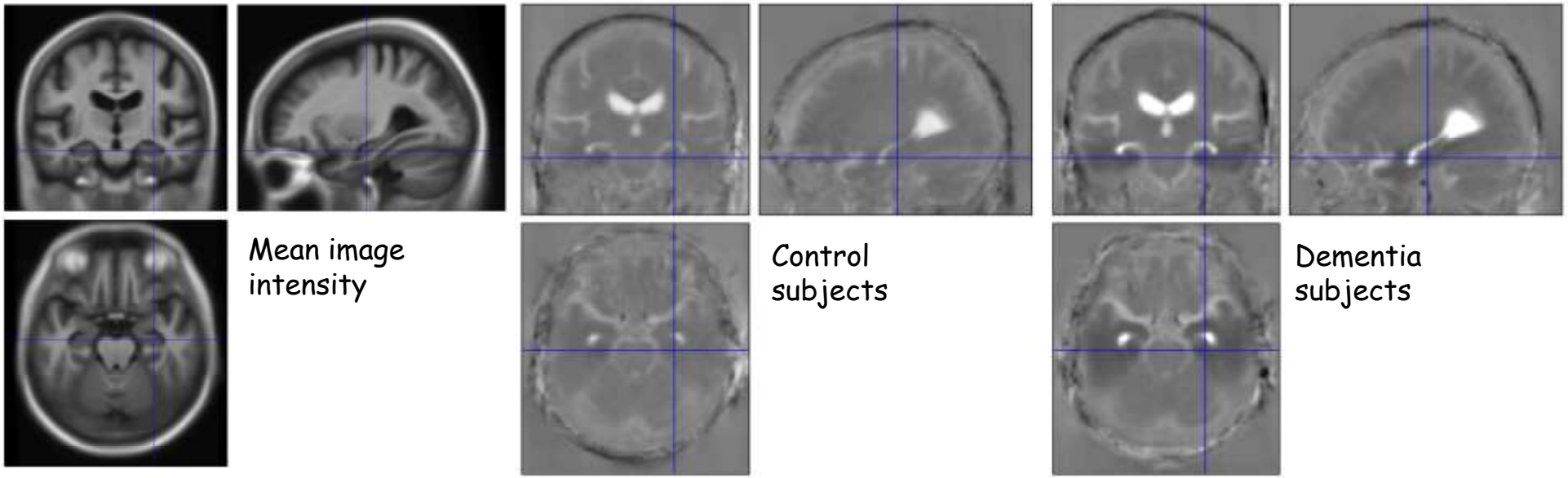
Oasis Data

Data from first 82 subjects (OAS2 0001 to OAS2 0099).

Computed average expansion/contraction rates for each subject.

Warped all data to common anatomical space.

Generated averages.



References

- Ashburner & Ridgway (2013). *Symmetric diffeomorphic modelling of longitudinal structural MRI*. Frontiers in Brain Imaging Methods 6(197).